

Accelerators For Medicine: Achievements, Challenges, Opportunities

Jürgen Debus

Department Radiation Oncology, Univ. Heidelberg
and Heidelberg Ion Therapy Center, Germany

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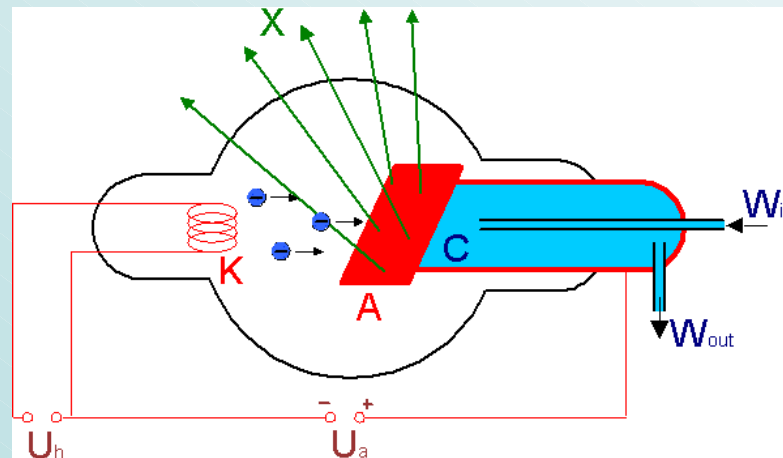
History of medical applications of accelerators

- 1895 *Wilhelm Conrad Röntgen* (1845 – 1923) discovers the X-rays on 8th November at the University in Würzburg
- 1896 On 23rd January Röntgen announced his discovery and demonstrated the new kind of radiation by a photograph of the hand of his colleague *Albert von Kolliker*
- 1897 First treatments of tissue with X-rays by *Leopold Freund* at University in Vienna
- 1901 Physics Nobel prize for W.C. Röntgen



Die durchleuchtete Hand von Bertha Röntgen 1895. Sie gilt als erste Röntgenaufnahme von einem Menschen.

Schematics of an X-ray tube – an “electrostatic accelerator”



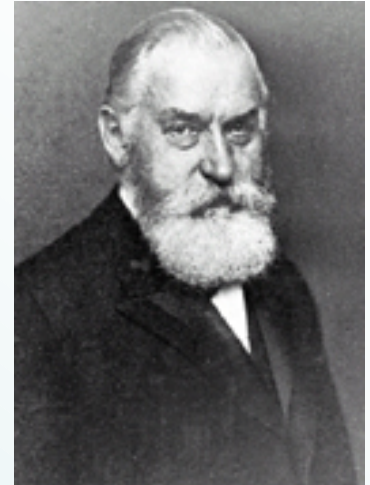
History:

High Voltage Therapy Of Cancer Heidelberg, 1907

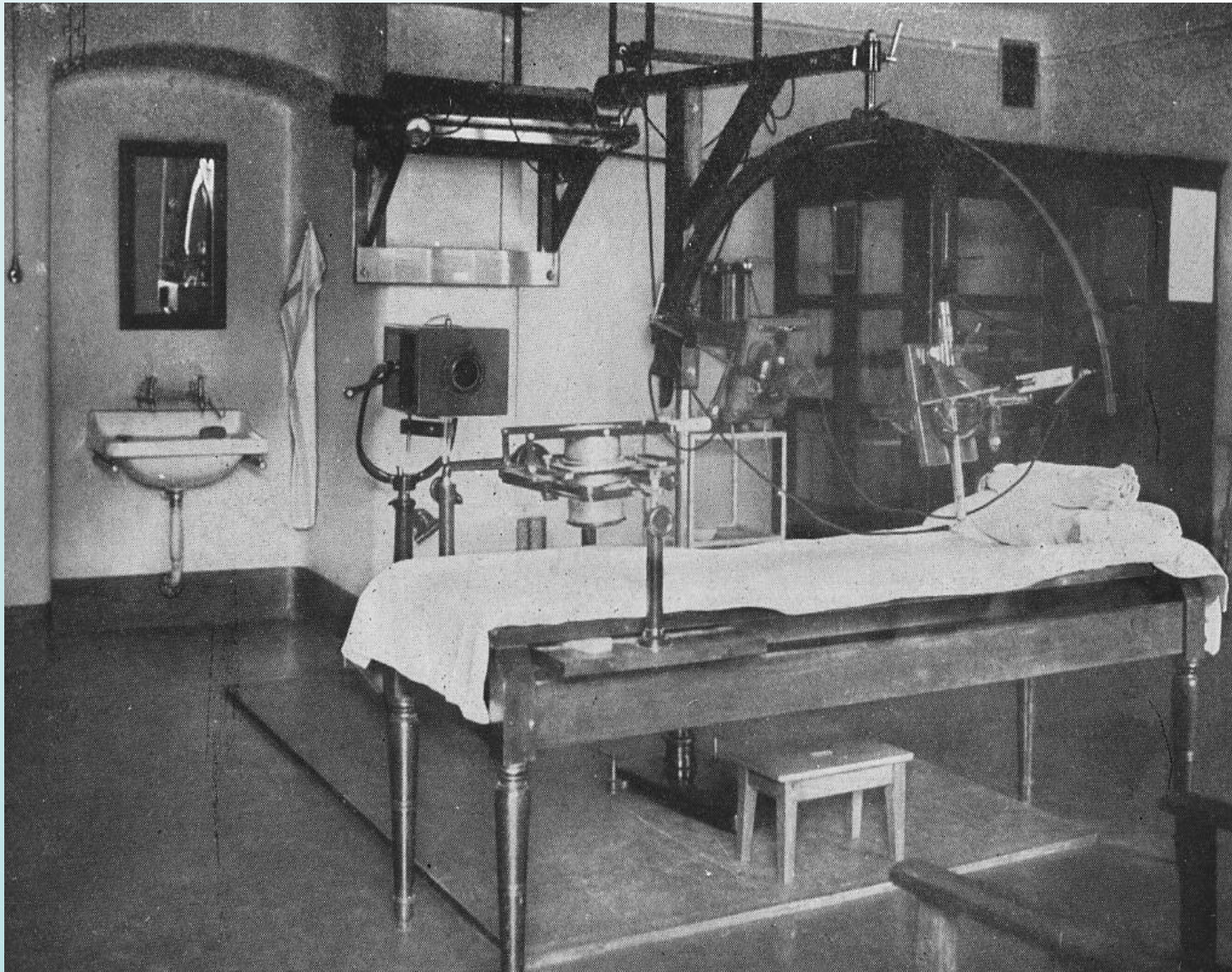


History of medical applications of accelerators

- 1899 First X-ray treatment of carcinoma in Sweden by *Stenbeck* and *Sjögren*
- 1906 Vinzenz Czerny founded the “Institute for Experimental Cancer research” in Heidelberg – the first of its kind
- 1913/4 Invention of part- and full-rotation radiation instrumentation
- 1920´ s Industrially manufactured X-ray apparatus; example from Reiniger-Gebbert & Schall AG (later: Siemens), Erlangen; 1922) with a high-voltage of 150 kV – without shielding!
- 1930 First linear accelerator principle invented by *Rolf Wideroe*
- 1949 *Newberry* developed first linear accelerator for therapy in England



Radiation „Concentrator“, Heidelberg 1913

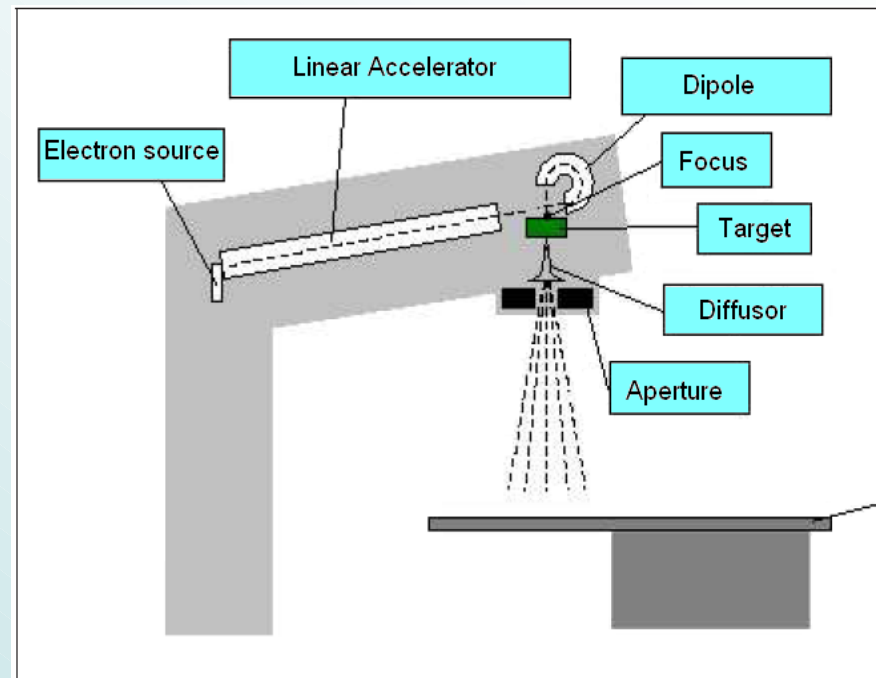


History of medical applications of accelerators

1950's Development of compact linear accelerators by
and Varian, Siemens, GE, Philipps and others
later with energies up to around 25 MeV (and above)



radiotherapy (Stanford linac)

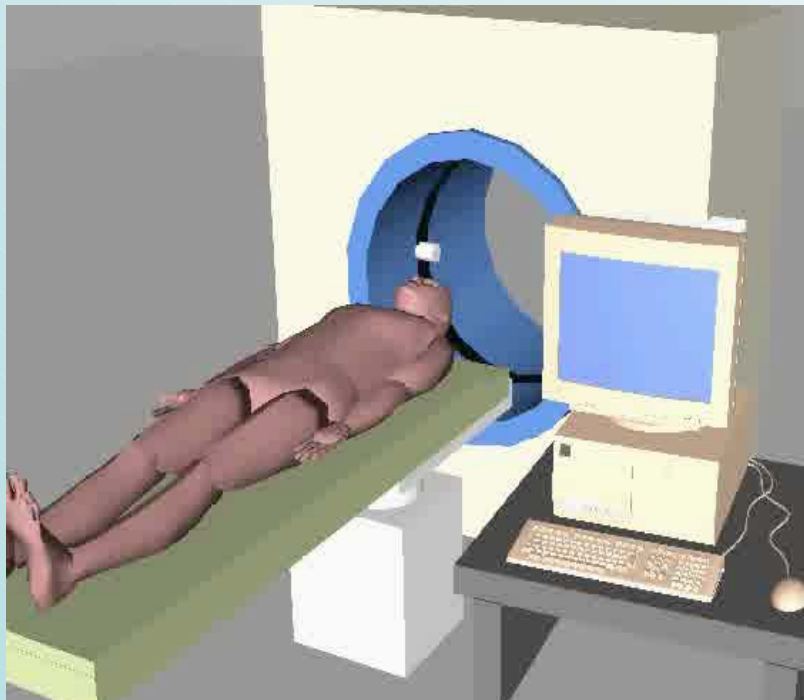


modern linac for therapy

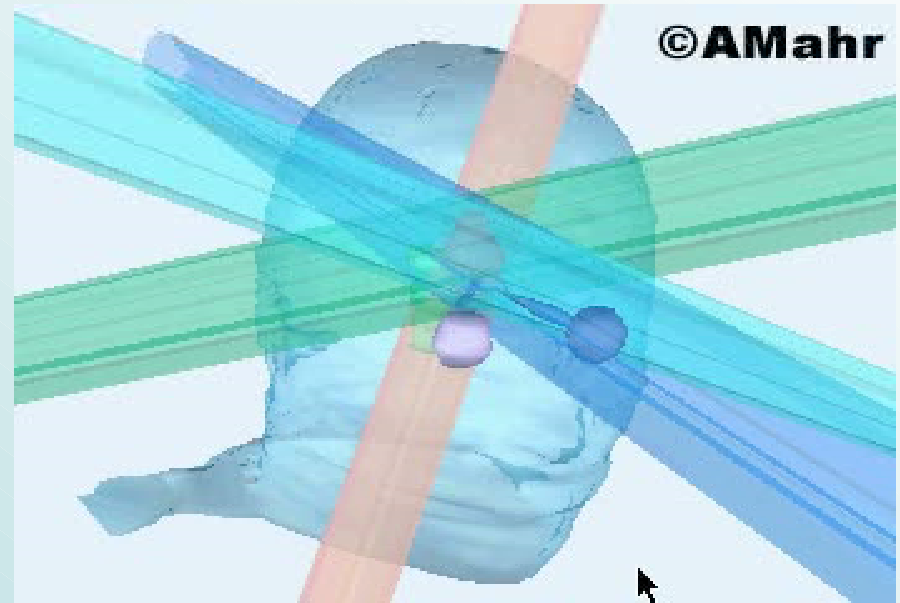
Treatment Planning:

Identify the target, model the patient, model the beam

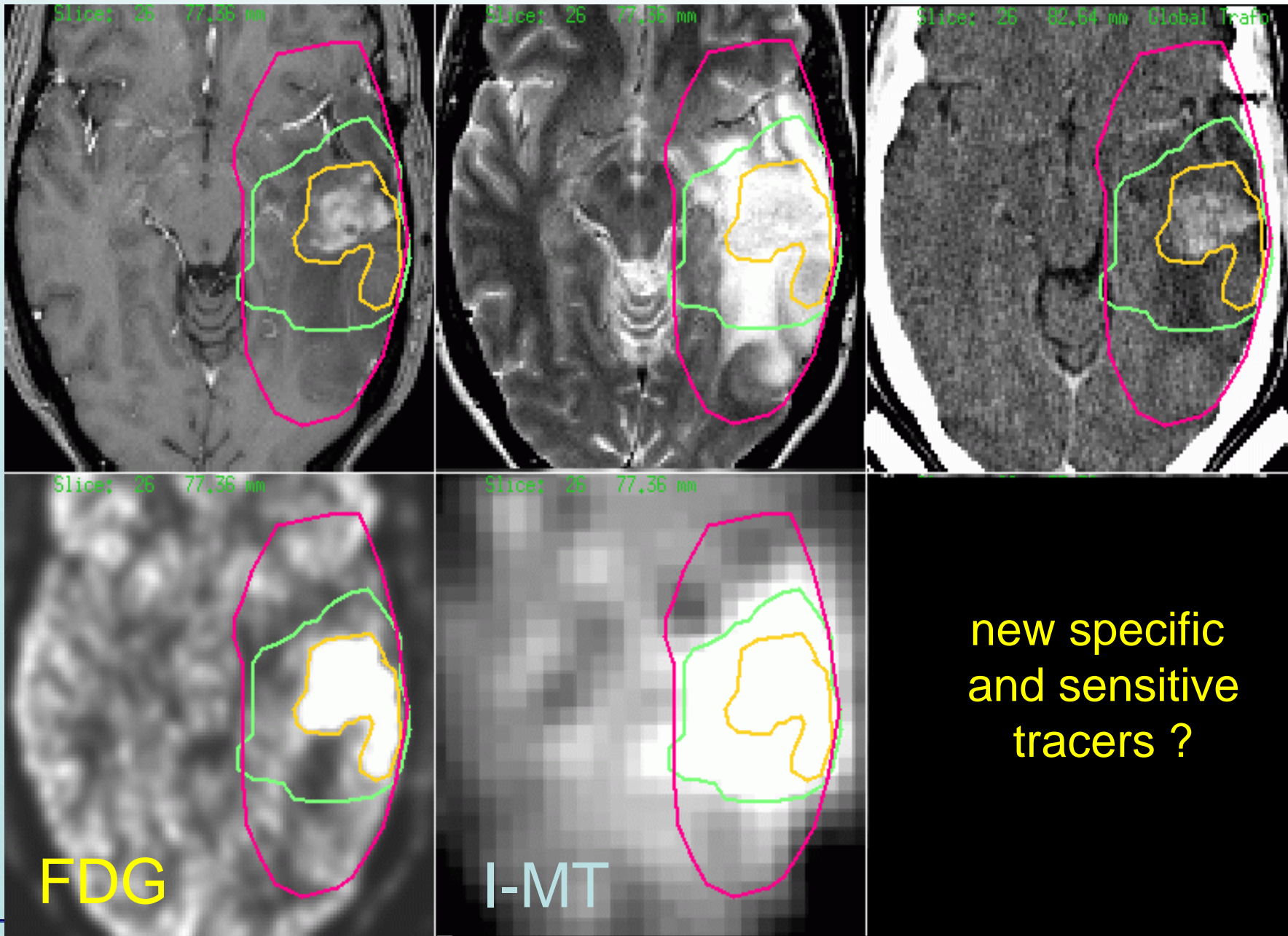
1. model of the patient



2. model of the beam



Target Definition By Multi-Modal Imaging: Glioblastoma



PET Tracers In Oncology: Molecular Imaging

Metabolism

^{18}F FDG

^{18}F FECh

Amino acids

^{11}C -methionine

^{18}F -tyrosine

^{11}C -AIB

^{18}F FET

Peptides

^{68}Ga -DOTATOC

Angiogenesis

^{18}F -Galacto-RGD

Perfusion

H_2^{15}O

Proliferation

^{11}C -thymidine

^{18}F FLT

Hypoxia

^{18}F -MISO

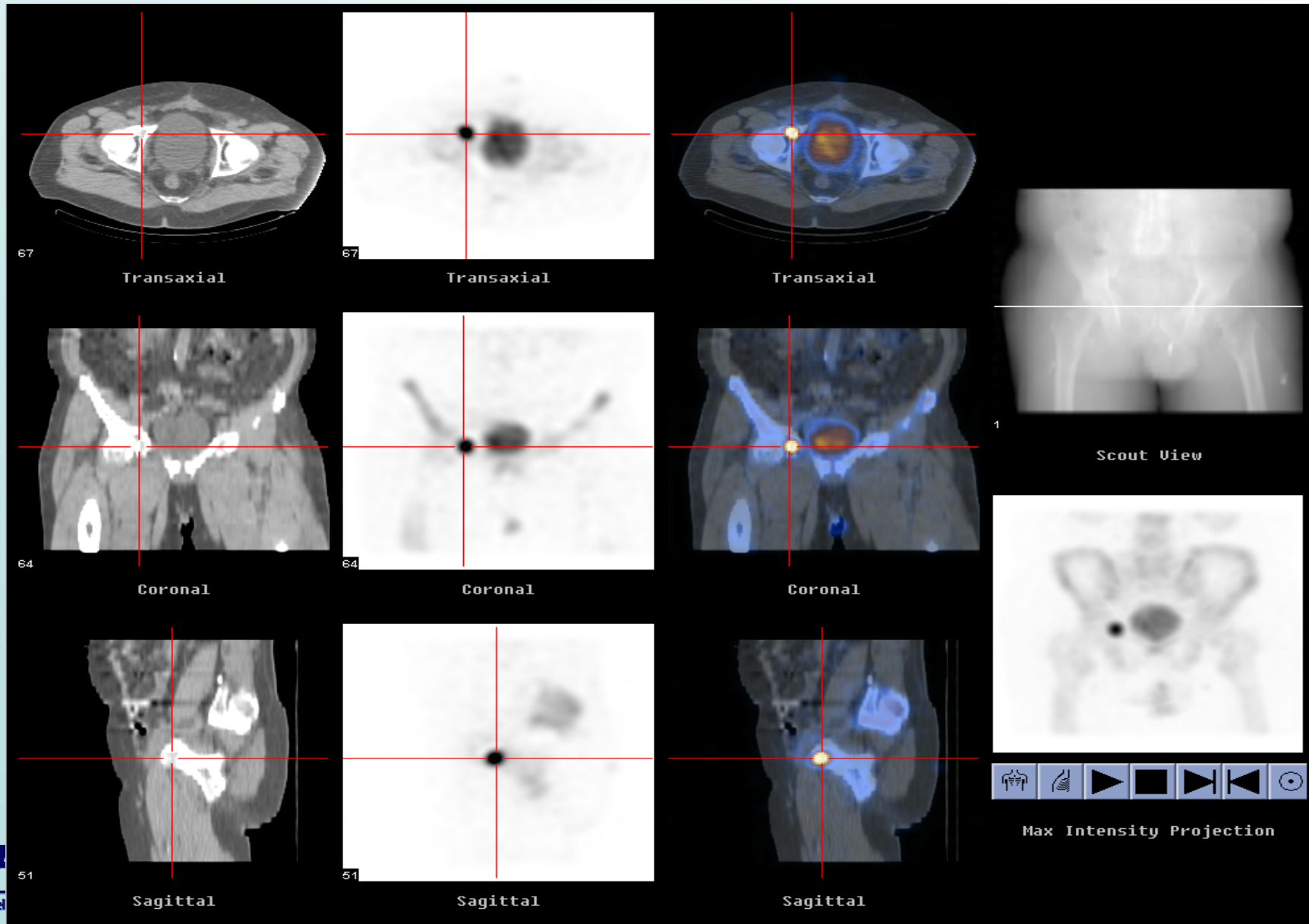
Drugs

^{18}F FU

many others experimentally

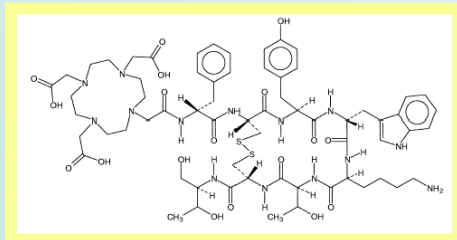
apoptoses, gen transfer etc.

Sensitive Imaging Of Tumors: FECH PET In Recurrent Prostate Cancer (PSA 1,4)

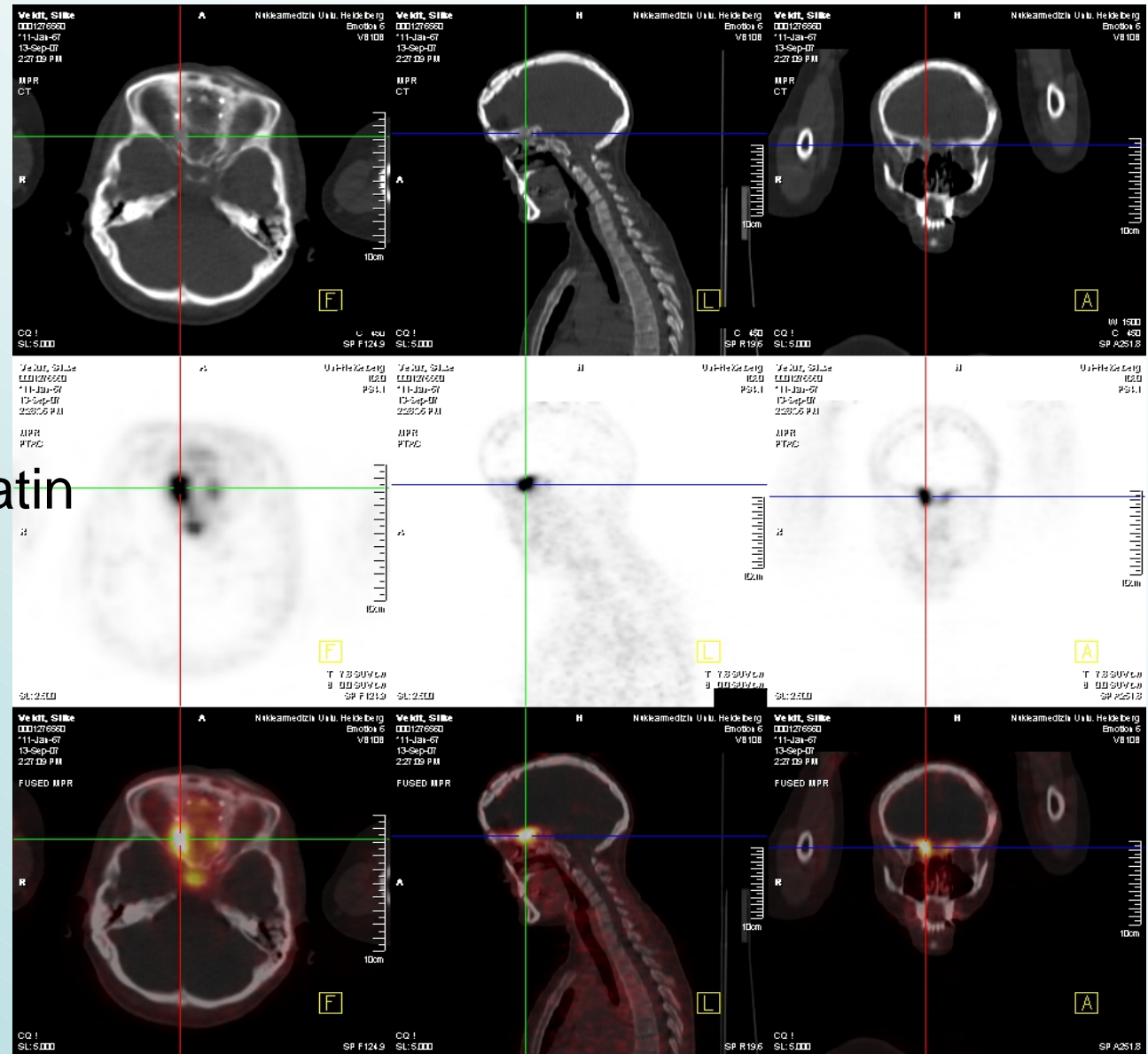


Imaging For RT Planning With DOTATOC: Recurrence Of Olfactorius Meningeoma

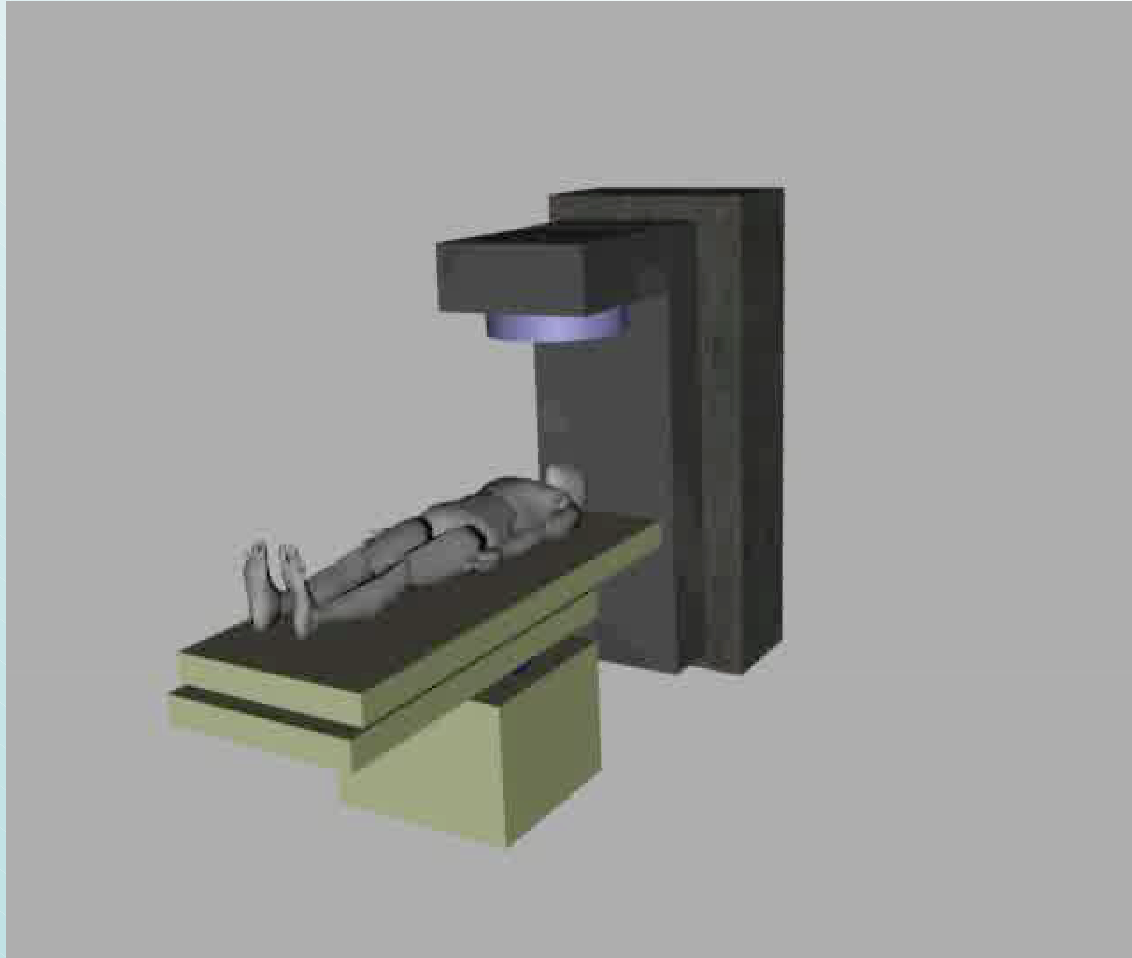
^{68}Ga -DOTATOC



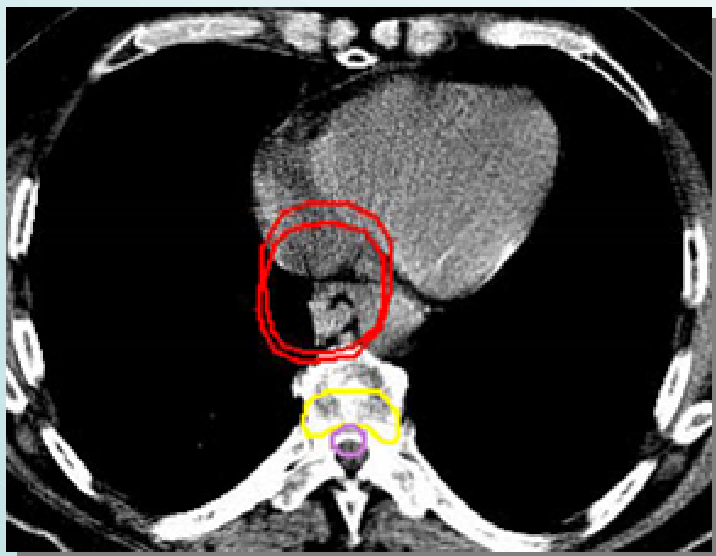
Binds to somatostatin
receptor type II



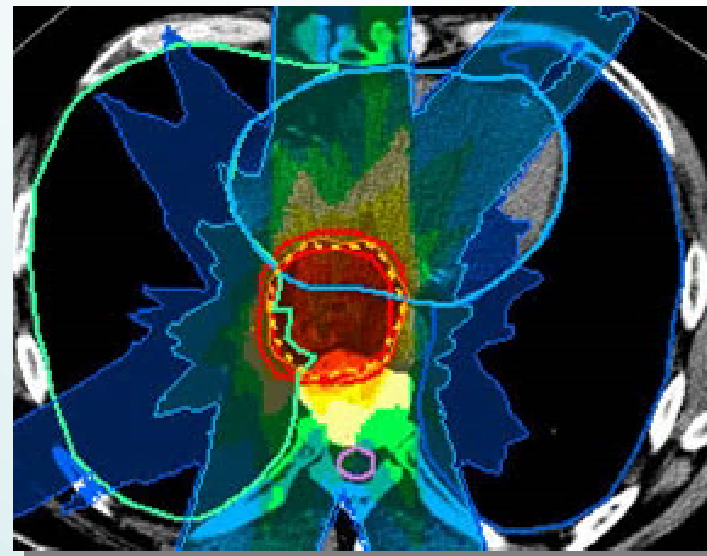
Intensity Modulated Radiotherapy (IMRT)



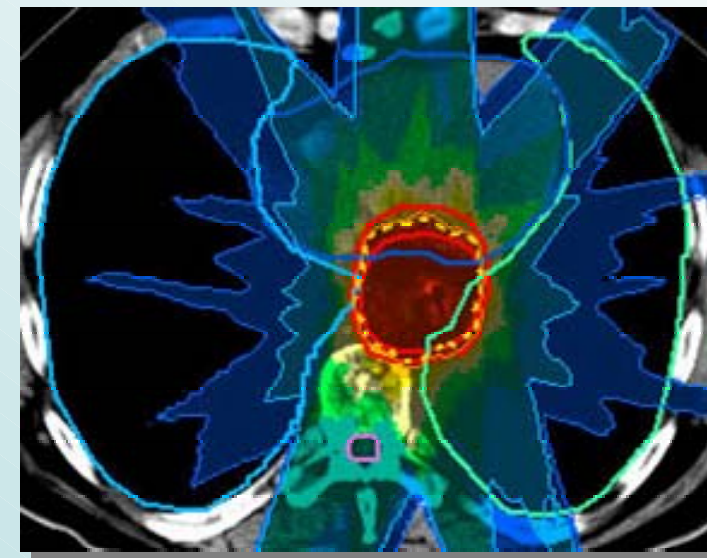
Esophageal Cancer: Potential Variation Of The Target



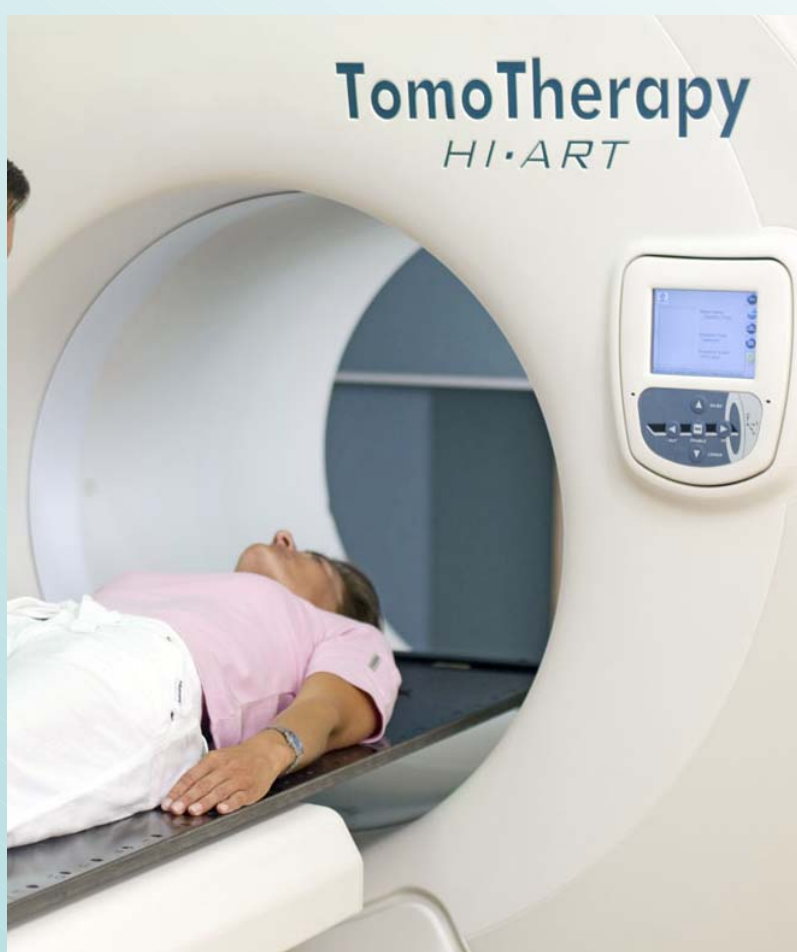
Var. 1:
9 days



Var. 2:
11 days

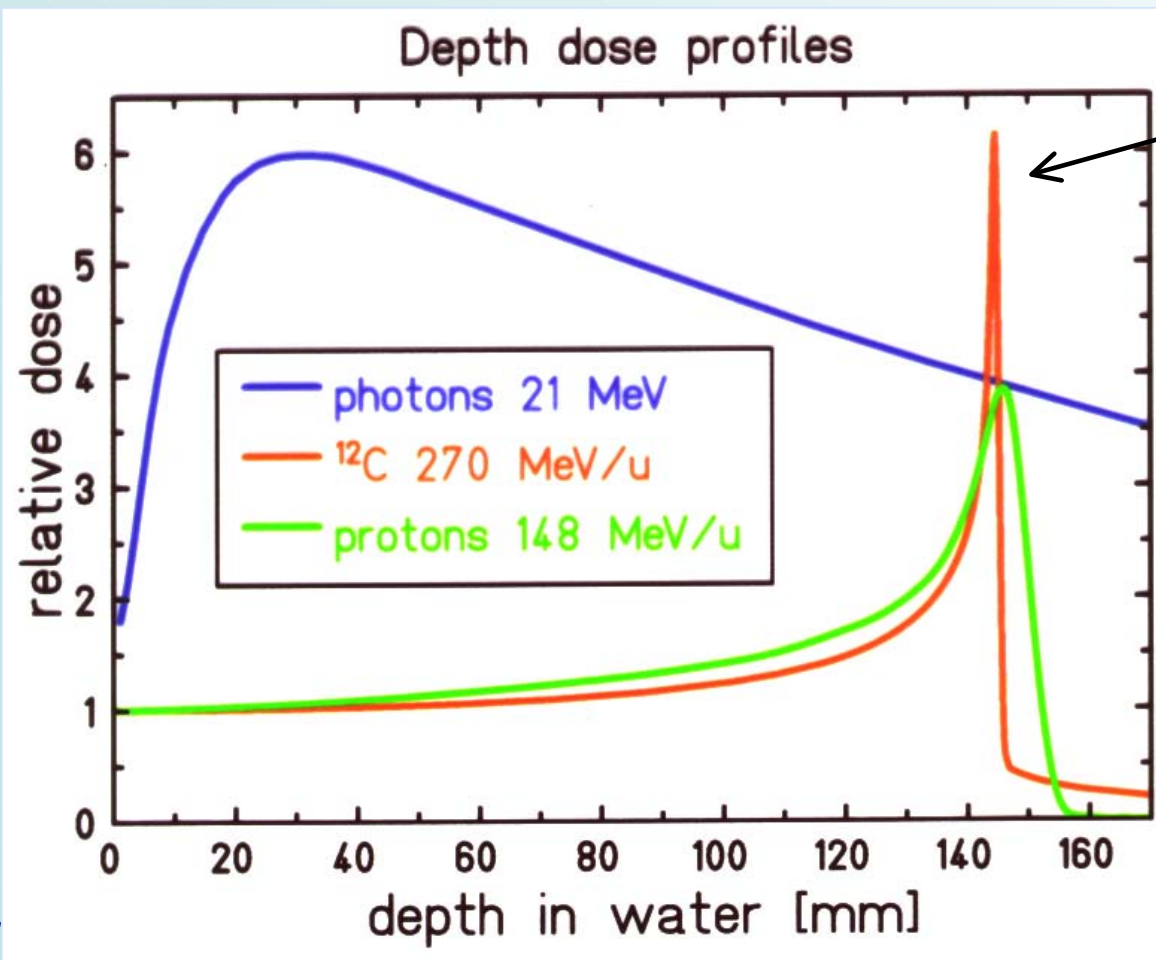


Integration Of Imaging And Treatment



- combination of CT-scanner and linear accelerator
- 85 cm Gantry-opening
- radiation volume
 - diameter up to 40cm
 - length up to 160cm
- 6 MV photons
- megavoltage CT (3MV)

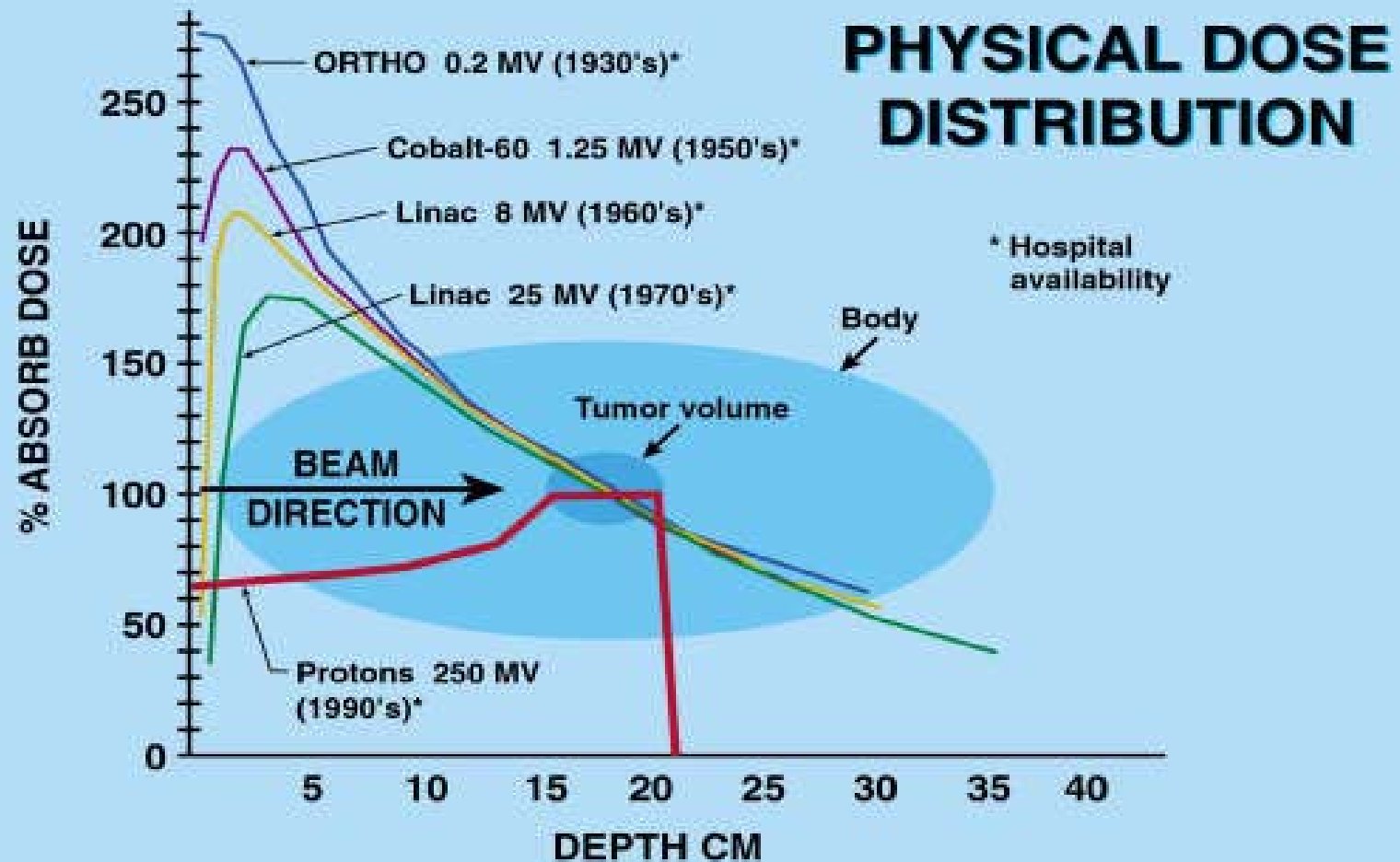
Charged Particle Beams Slow Down And Stop X-rays keep going at the speed of light



„Bragg“-peak

Heavy Charged Particles In Radiotherapy

It's simply the physics!



History of medical applications of accelerators

1929 Invention of cyclotron by *Ernest Lawrence*

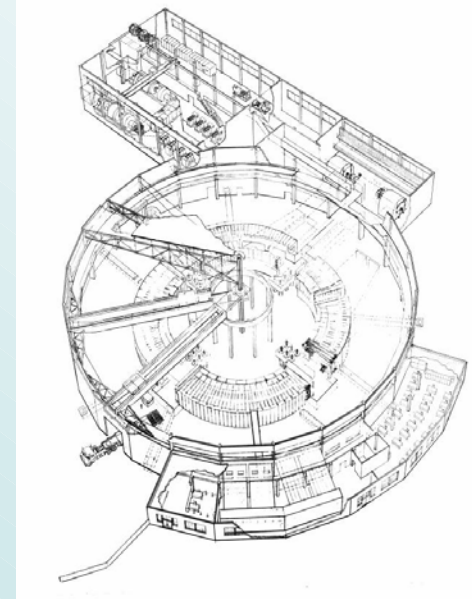
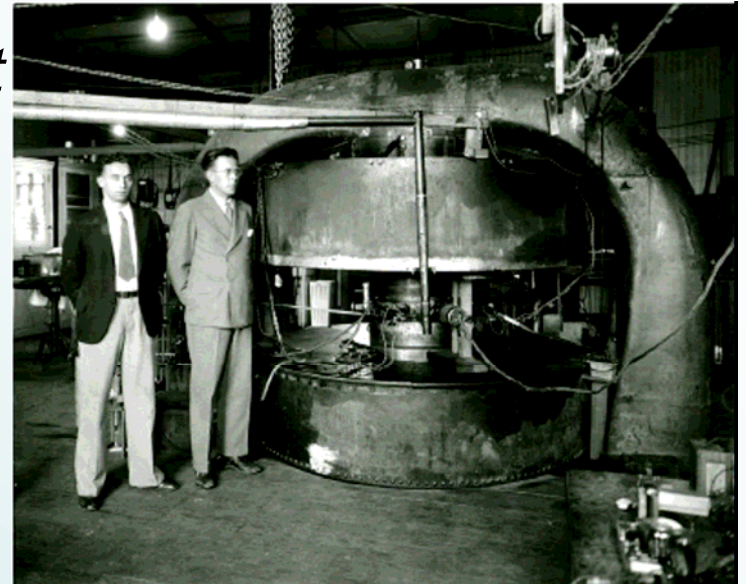
1930's Experimental neutron therapy

1946 R. R. Wilson proposed proton & ion therapy

1950's Proton therapy, LBL Berkeley (184" cyclotron)

1945 *Edwin Mattison McMillan* at University of California and *Vladimir Iosifovich Veksler* (Soviet Union) invented the synchrotron principle

1975 Begin of carbon therapy in Bevalac synchrotron (Berkeley)



Harvard Cyclotron: Patient Treatments 1974-2002

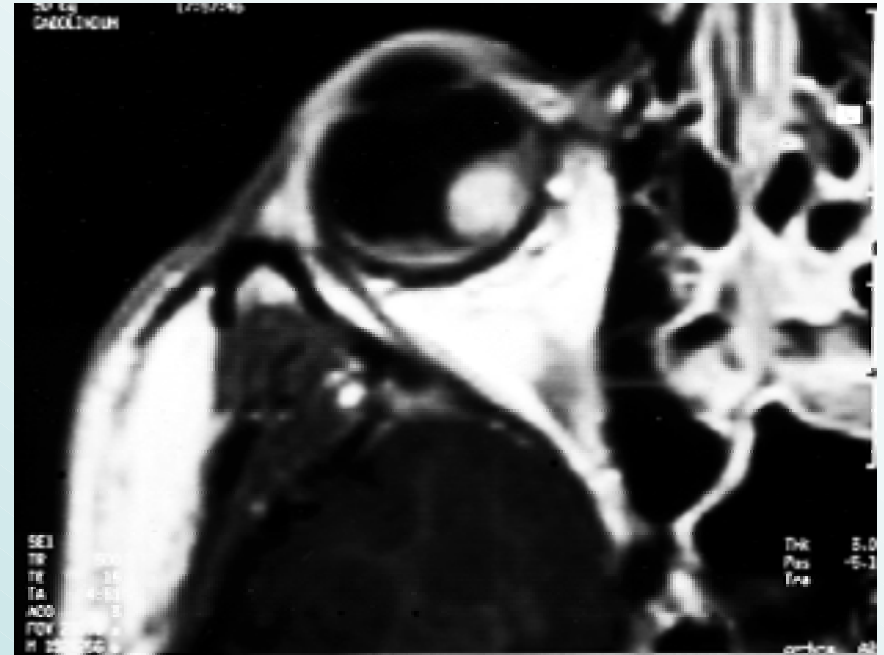


Treatment Of Ocular Melanoma At The Harvard Cyclotron



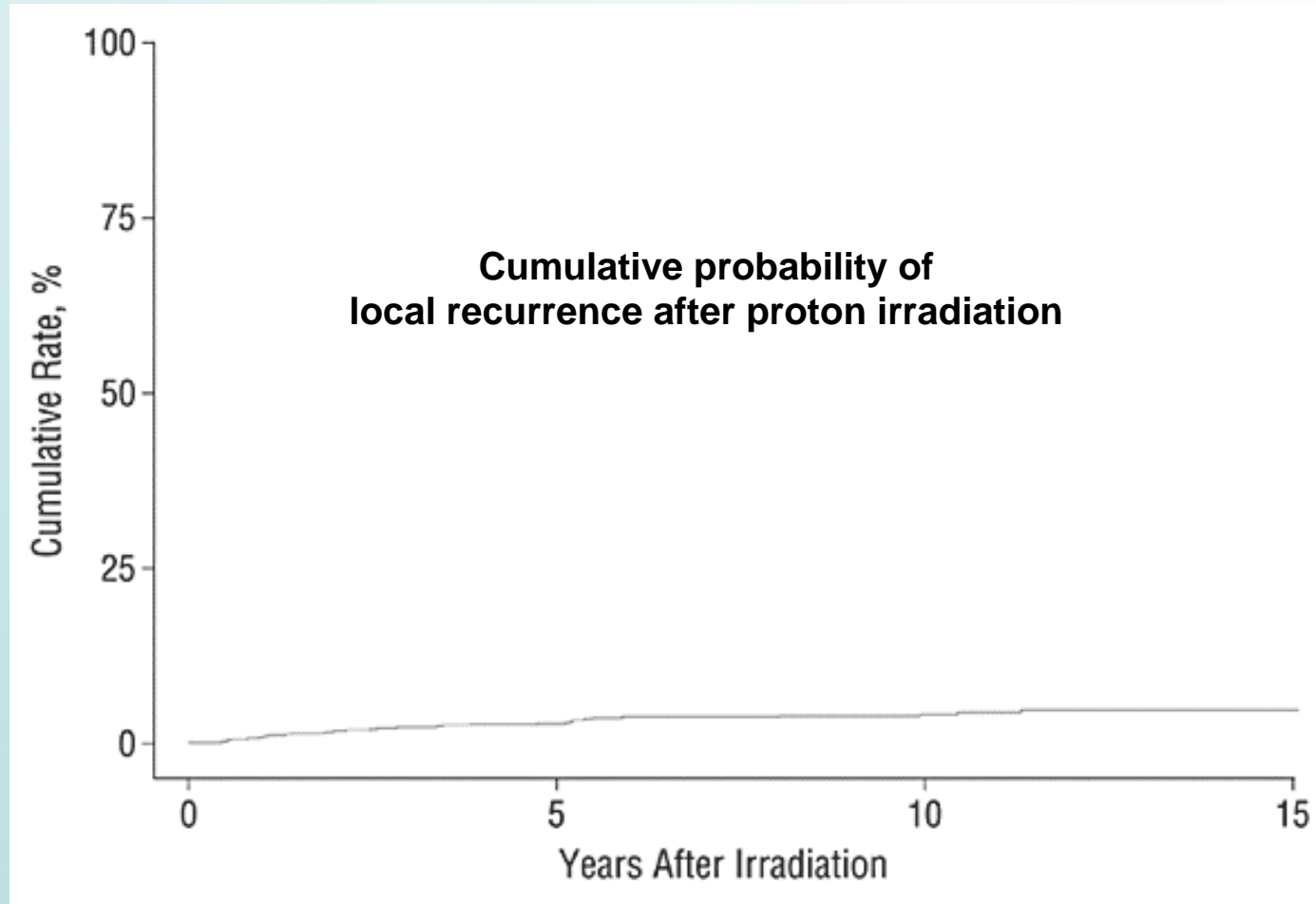
Occular Melanoma

Primary Symptom: reduced/disturbed vision



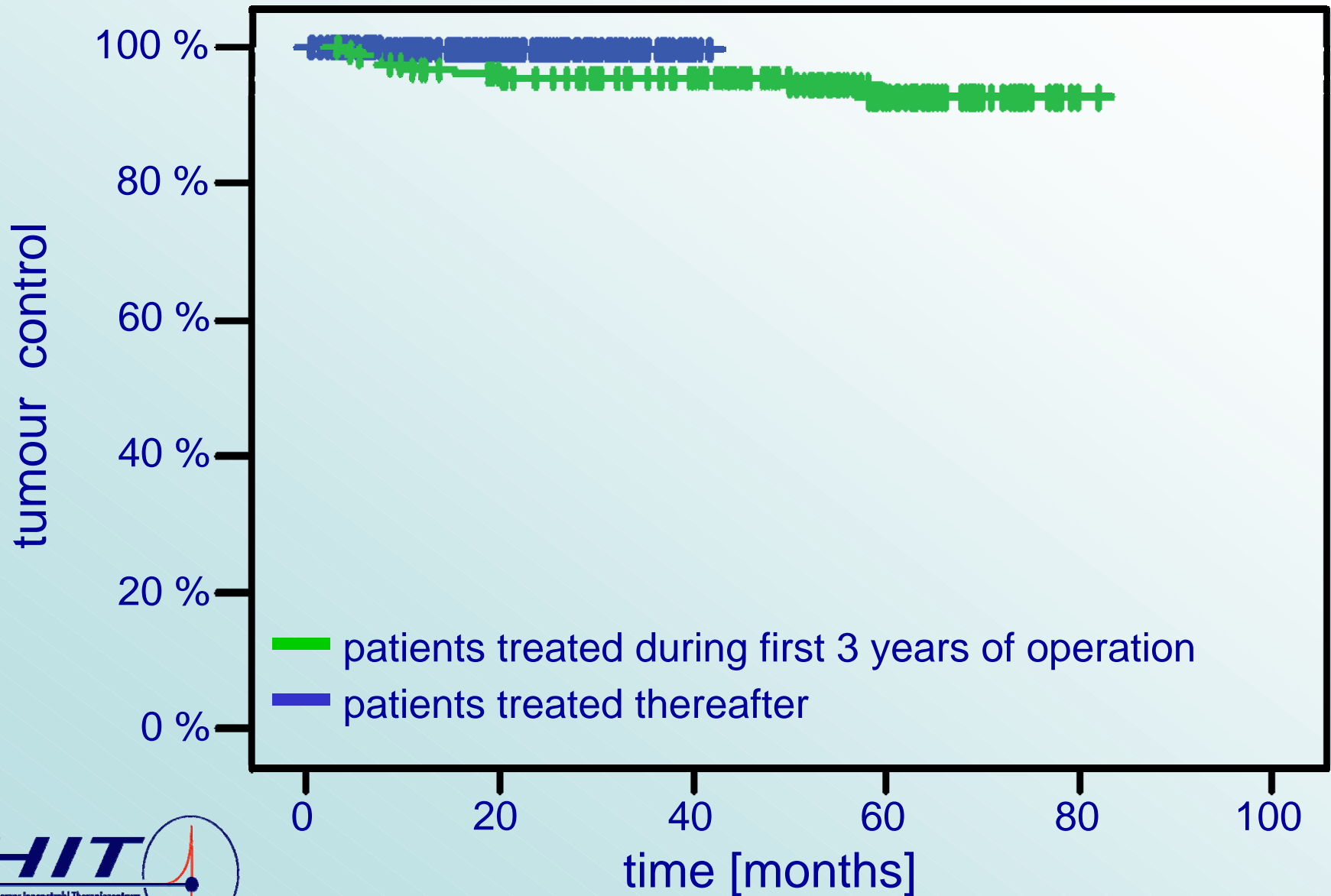
The MGH / MEEI Experience:

Gragoudas, E. et al. Arch Ophthalmol 2002;120:1665-1671.



Ocular Melanoma Proton Therapy at Hahn-Meitner Institute

The „Learning Curve“ (courtesy J. Heufelder)

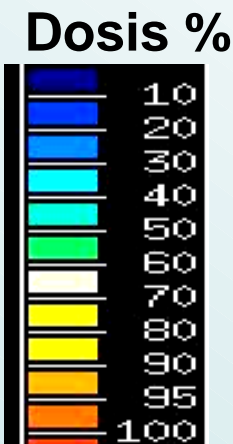
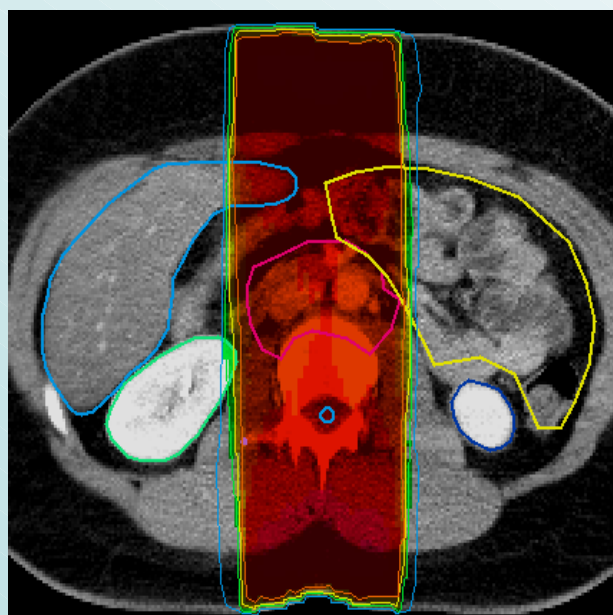


Potential Of Protons To Spare Uninvolved Structures

Radiotherapy Of Paraaortic Lymphnodes:

Challenge: Geometrical Changes During Treatment

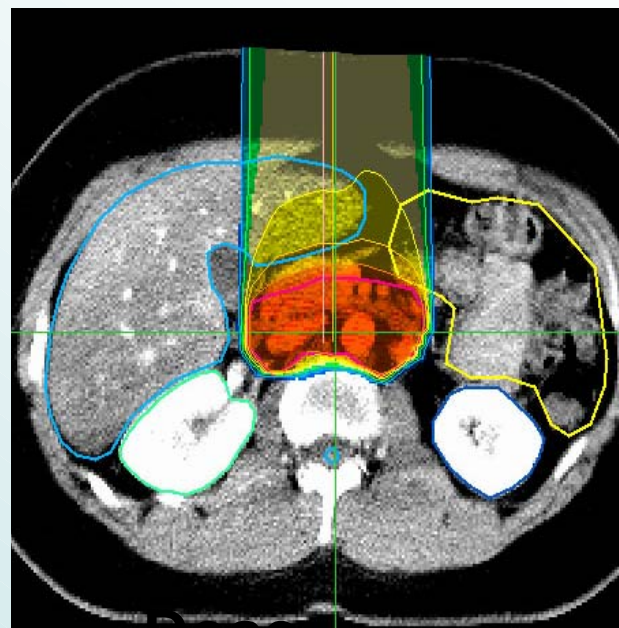
Conventional Approach



40 Gy
39 Gy
41 Gy

bone marrow
bowel
spinal cord
< 1 Gy

Particle Beams



Dose

< 1 Gy
26 Gy

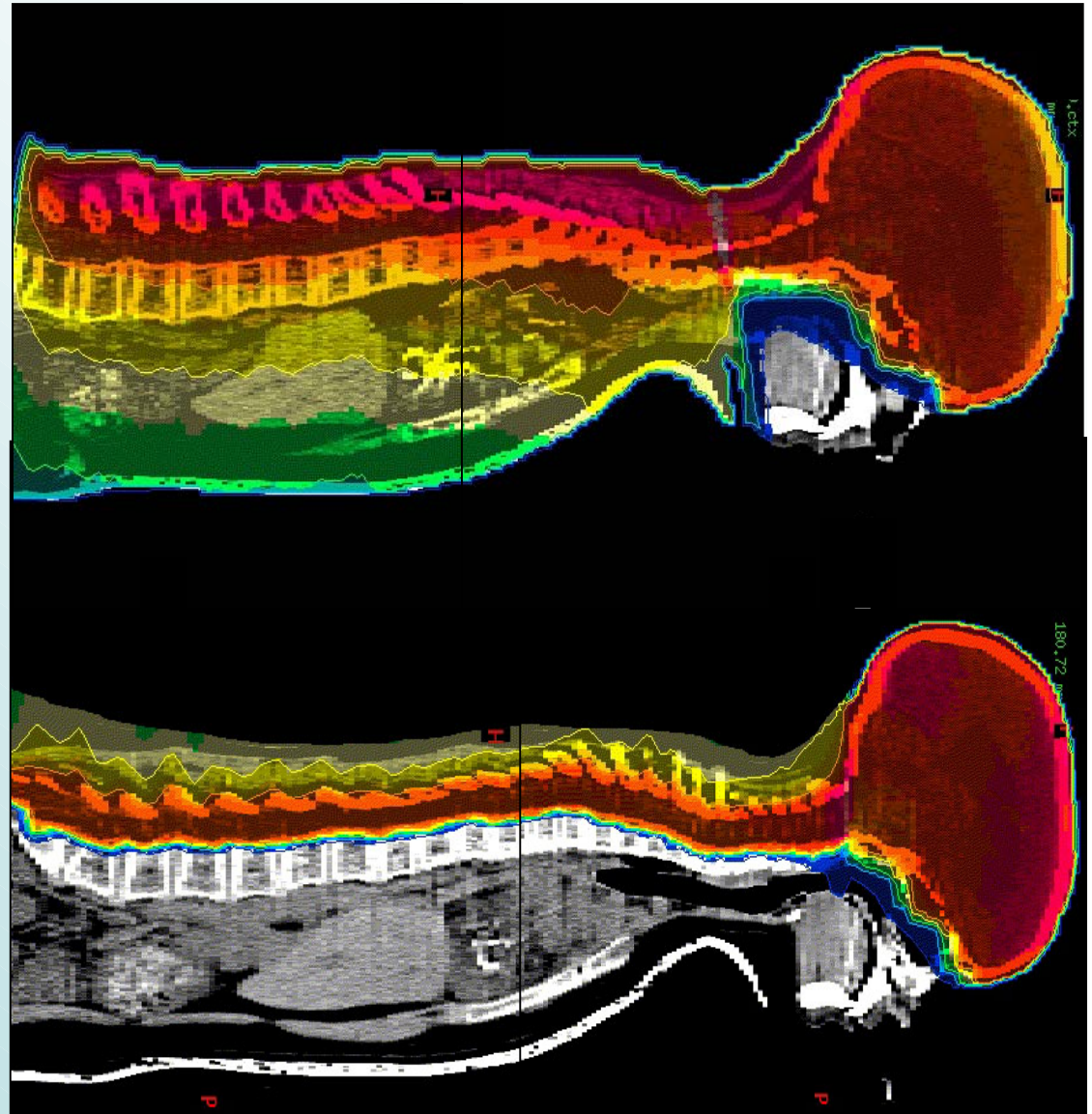
Craniospinal Radiotherapy For Medulloblastoma

charged particles can spare normal tissue

photons

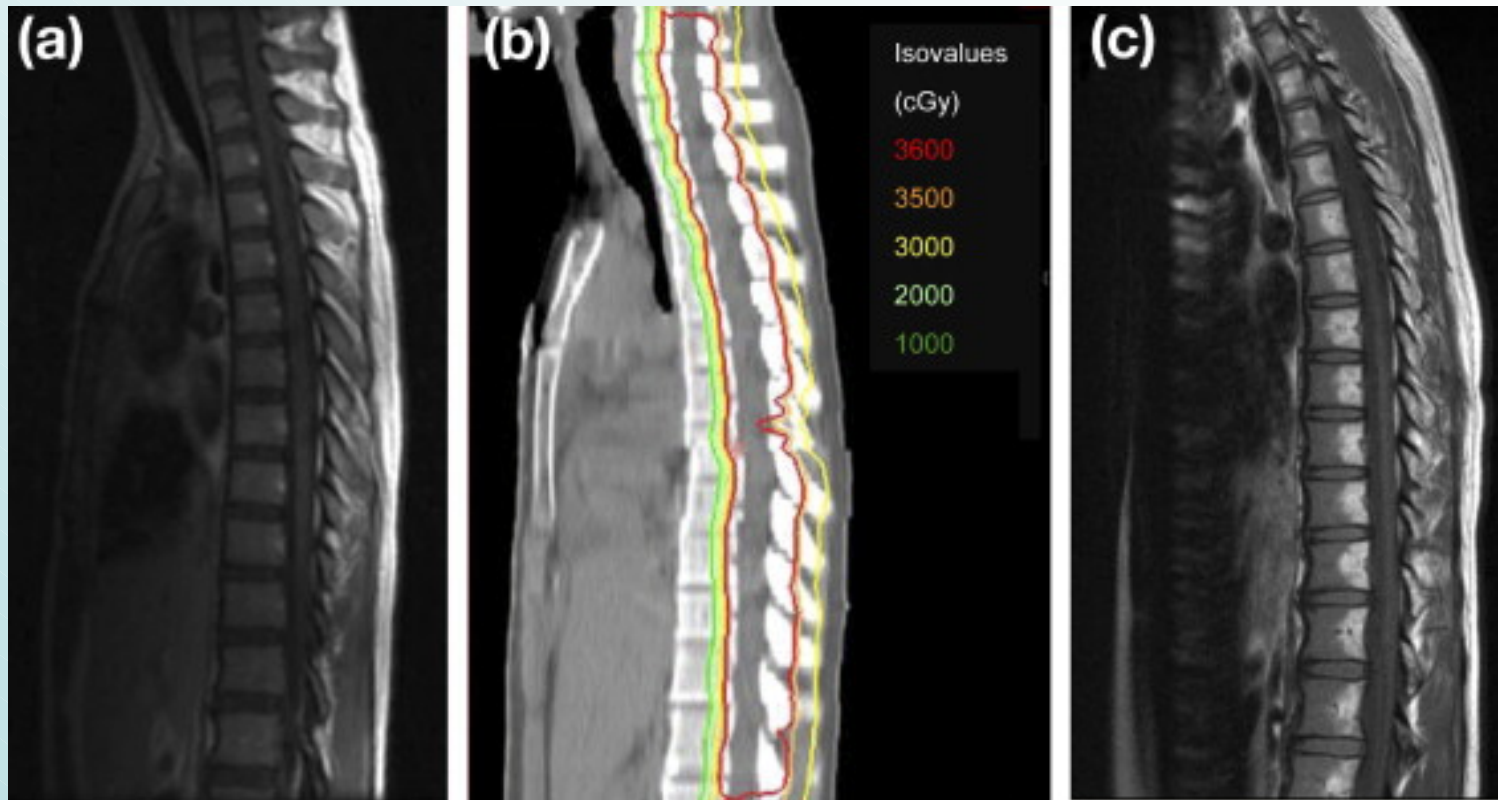
challenge:
size of the target !

particles



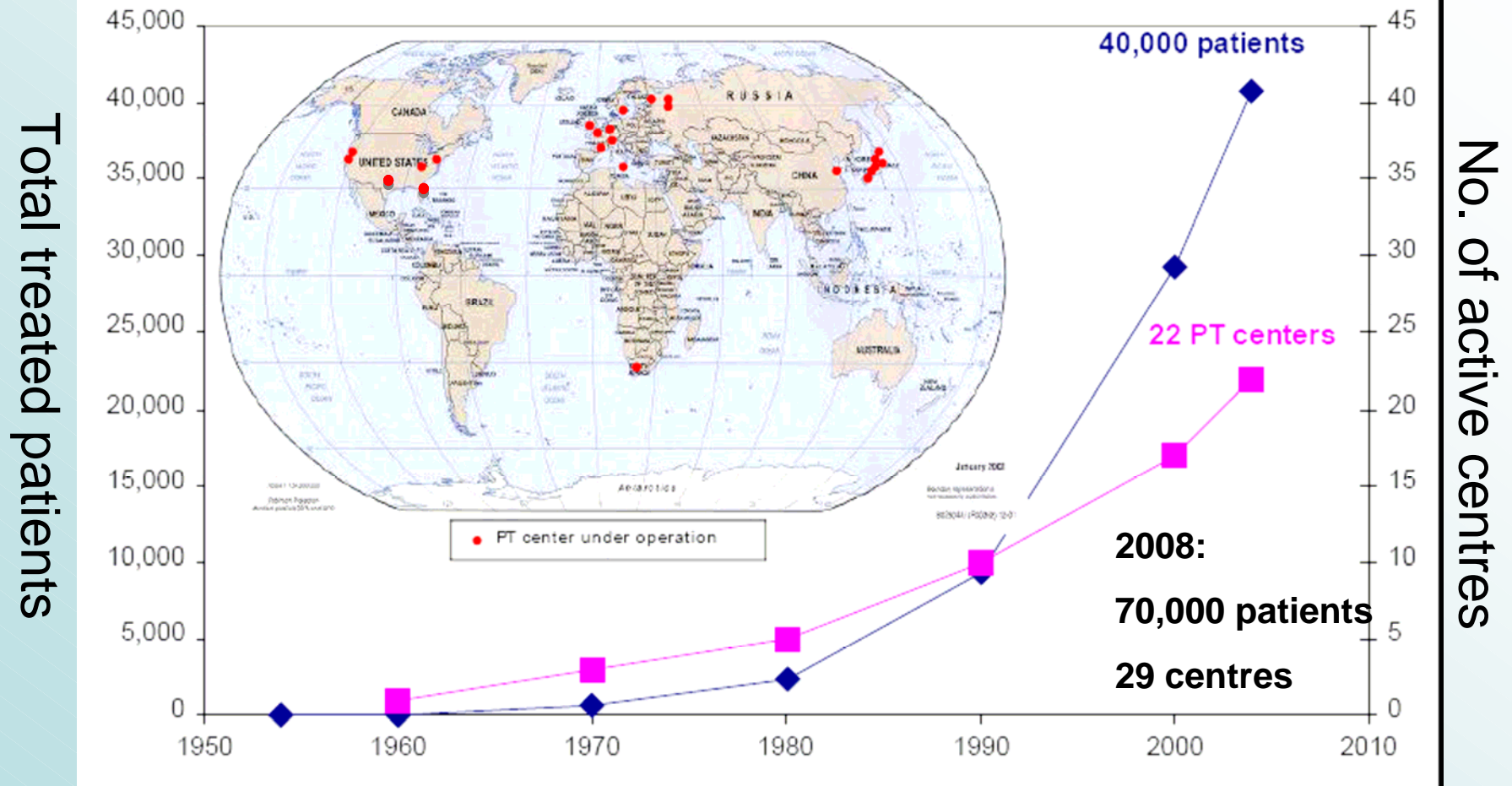
Craniospinal RT In 14 Year Old: Sparing Of Bone Marrow

Physiologic and Radiographic Evidence of the Distal Edge of the Proton Beam
in Craniospinal Irradiation Krejcarek SC, Tarbell NJ, Yock TI et al. IJROBP 68(3):646-649, 2007



A 14-year-old girl with supratentorial primitive neuroectodermal tumor: craniospinal irradiation prescribed to the thecal sac and exiting nerve roots only. (a) T1-weighted magnetic resonance image 1 week before radiation treatment. (b) proton radiotherapy treatment plan. (c) T1-weighted MRI with hyperintense fatty changes in posterior aspect of vertebral bodies 1 month after PRT.

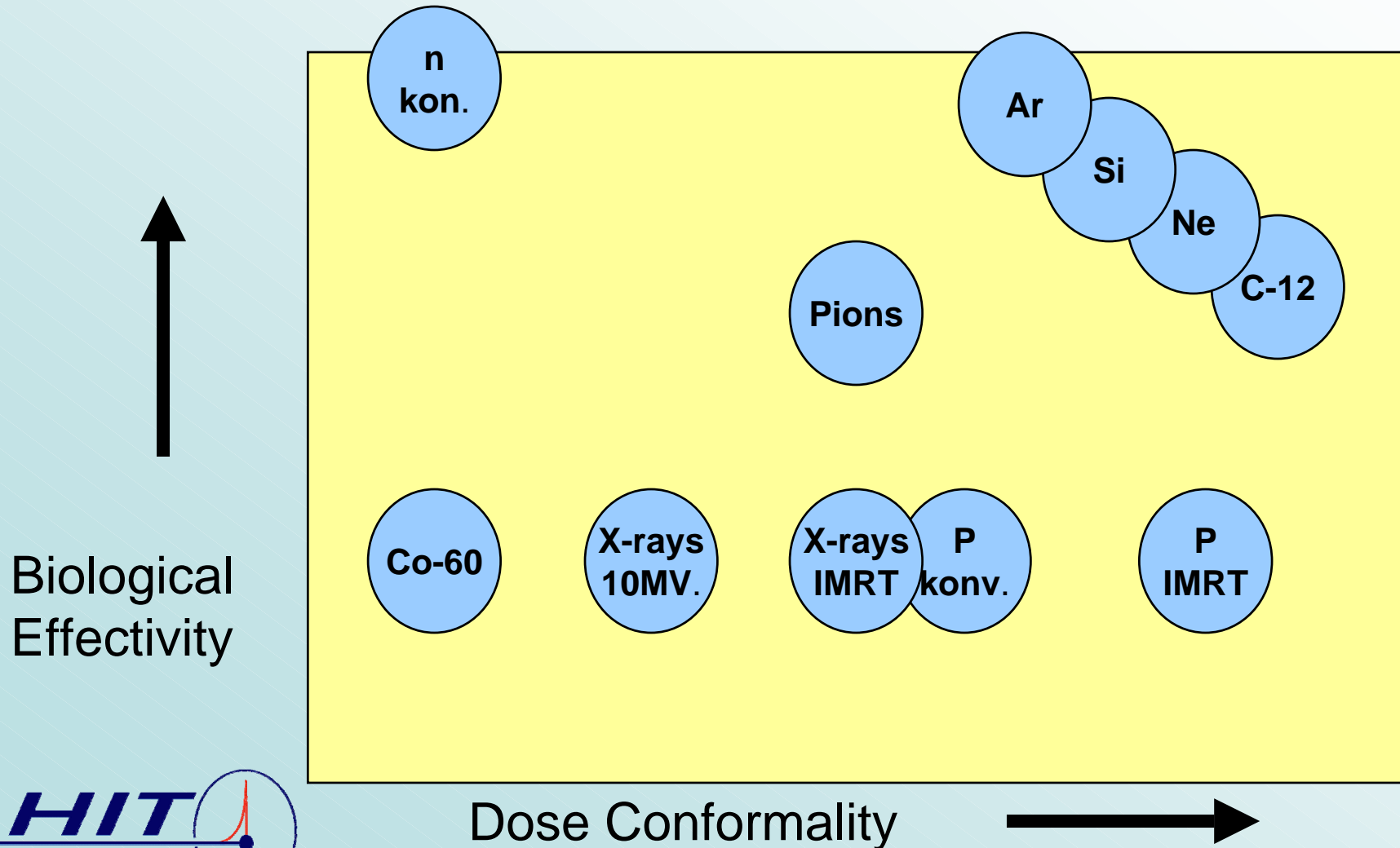
Particle Therapy Facilities - worldwide



PT centres: a rapidly growing market

Particles in Radiation Oncology

Comparison of Protons, Neutrons, Pions, Ions and Photons



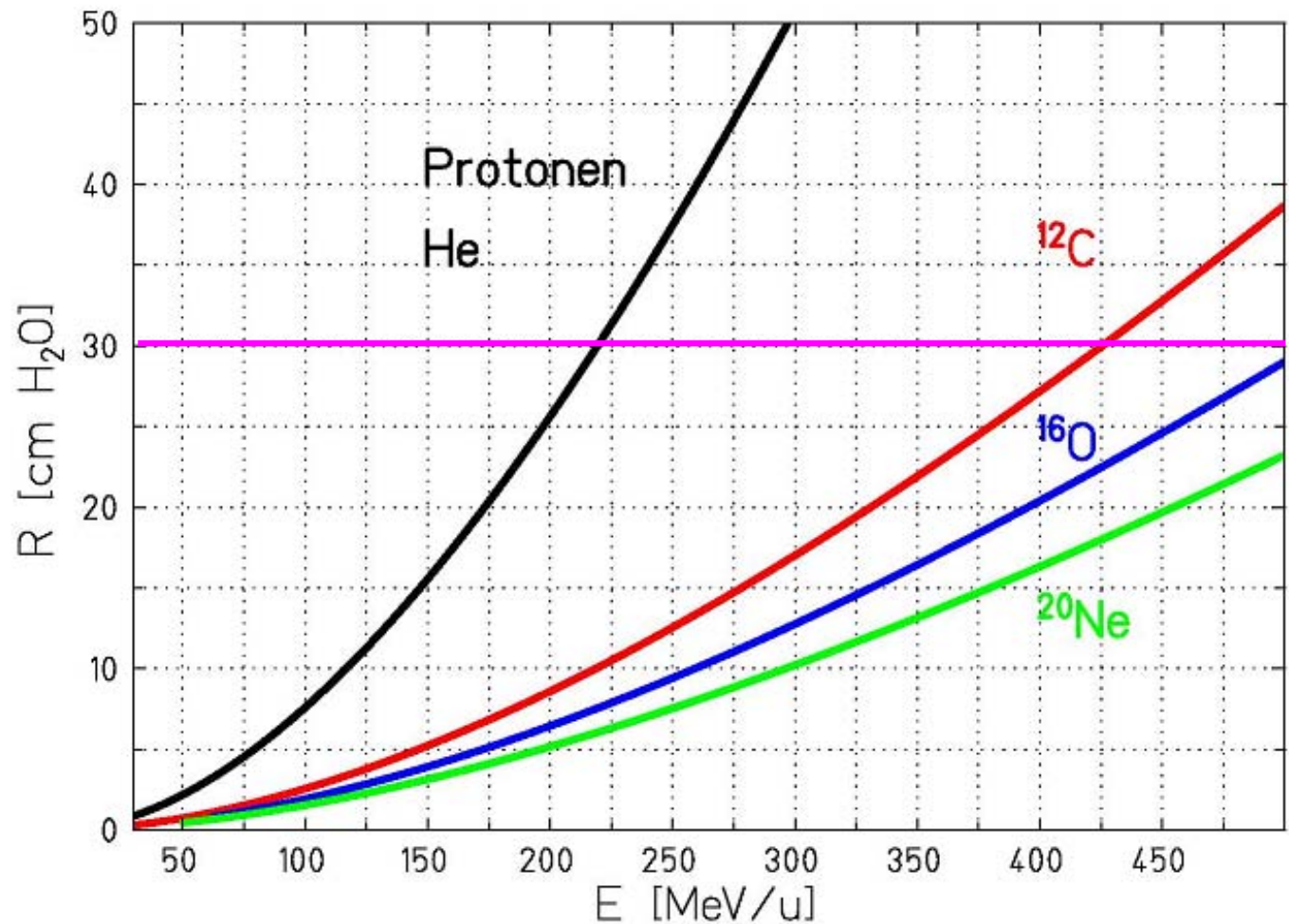
Implications on the beam energy

Range of different beams in water

30 cm range define the end energy for the accelerator design:

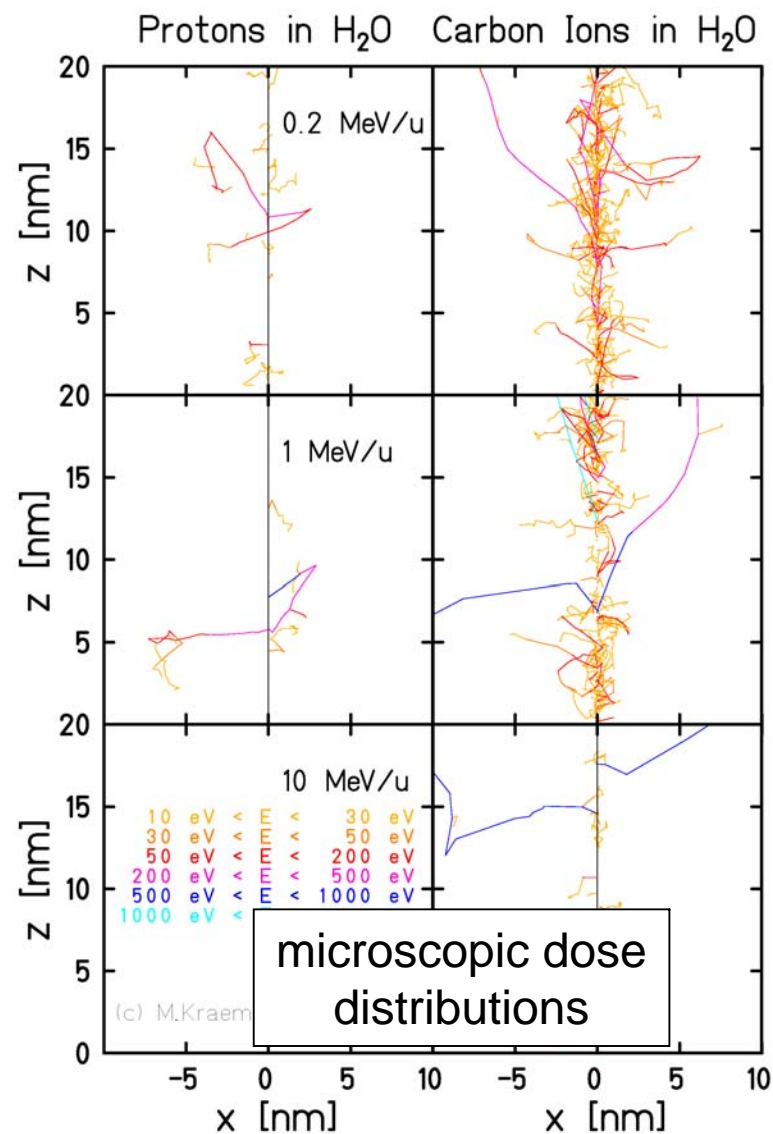
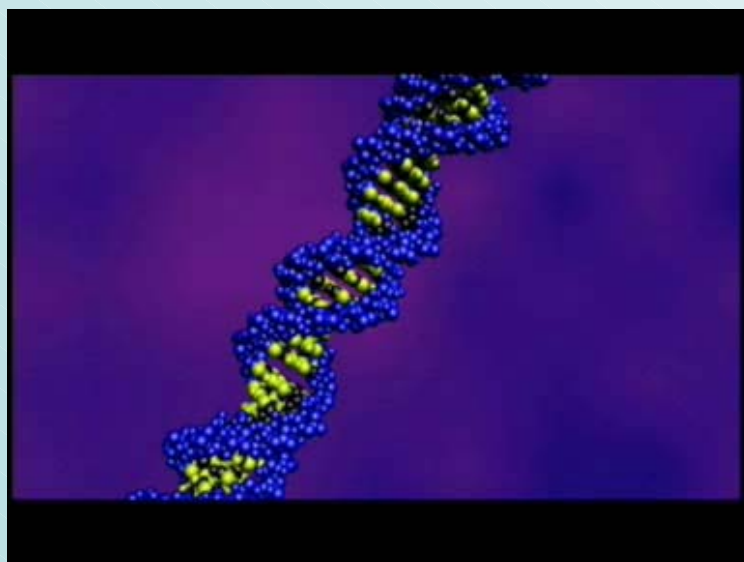
p → 220 MeV

C →
430 MeV/u

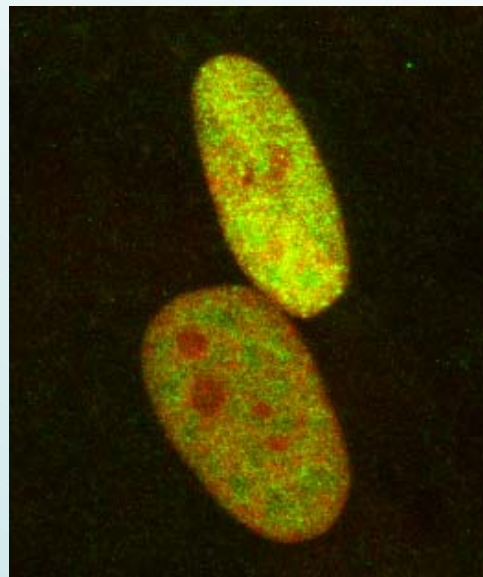
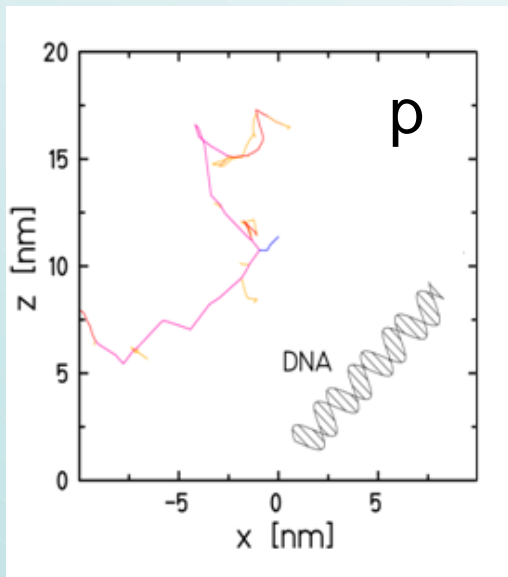


Physics and Biology of radiation therapy

Basic effect of radiation on cells: energy loss in matter leads to defects in the DNA – double strand breaks of the DNA kills the cell. Tumor cells have less repair capabilities than normal cells.

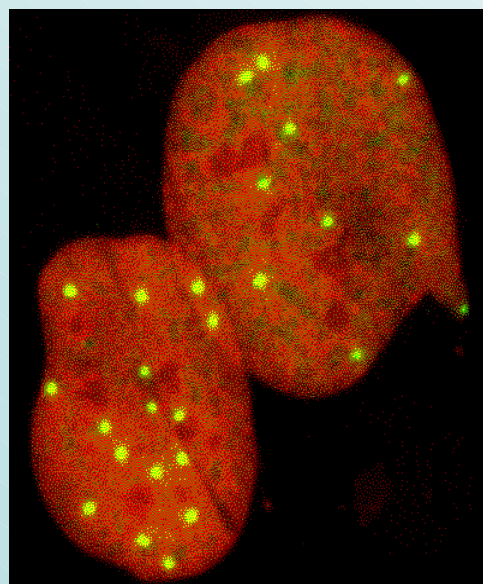
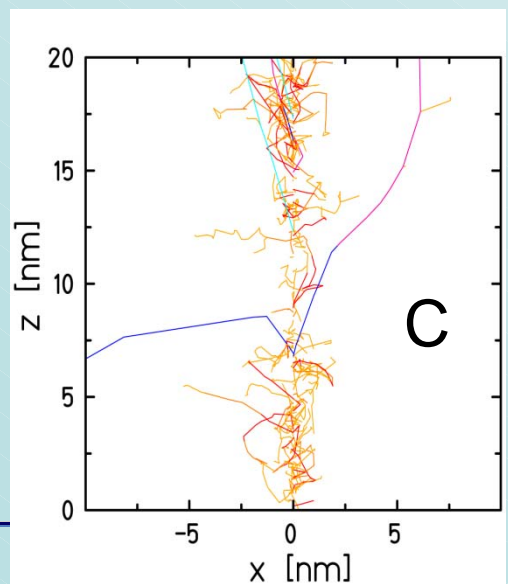


Physics and Biology of radiation therapy



Low LET

Homogeneous deposition of dose



High LET

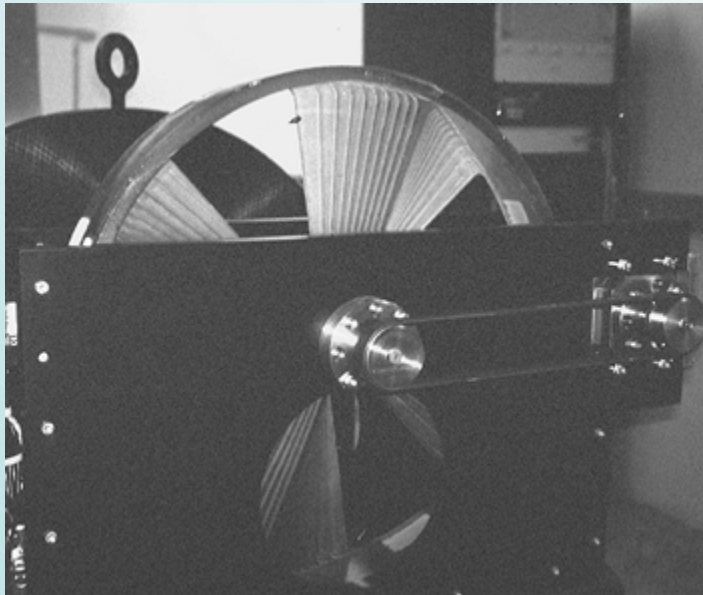
Local deposition of high doses

LET: Linear energy transfer

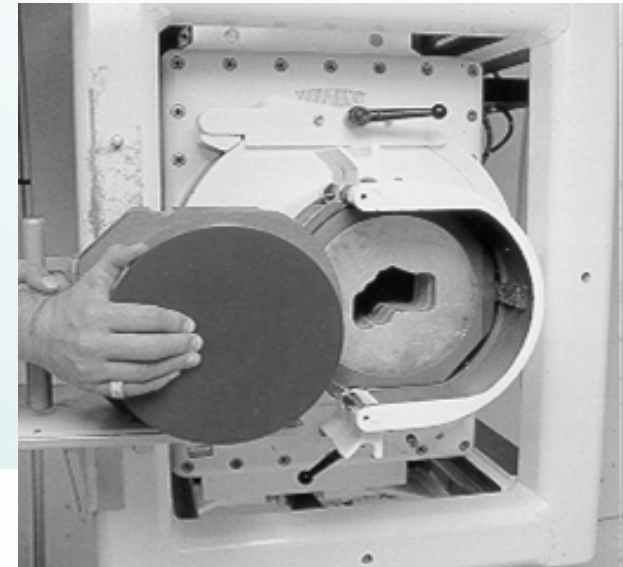
LBL, Berkeley, US Neon ion experience 1979-1998; 239 pts (Linstadt, 1991)

Tumor	# pts	Dose GyE (med.)	5y-LC	5y-DSS
Lung st. II-III	20	48-74 (63)	12 %	5 %
Esophagus	14	37-89 (68)	-	-
Stomach	9	45-60 (56)	37 %	11 %
Pancreas	64	30-71 (58)	6 % (3yrs)	1.5 % (OS)
Biliary tract	13	48-68 (60)	44 %	28 %
Prostate	12	70-79 (77)	75 %	90 %
Soft T. Sarcoma	12	37-80 (60)	56 %	56 %
Bone Sarcoma	19	50-76 (70)	59 %	45 %
Paran.sinus	12		69 %	69 %
Saliv. gland	18		61 %	59 %
Melanoma	6	48-80 (60)	-	-
Miscellaneous	40			

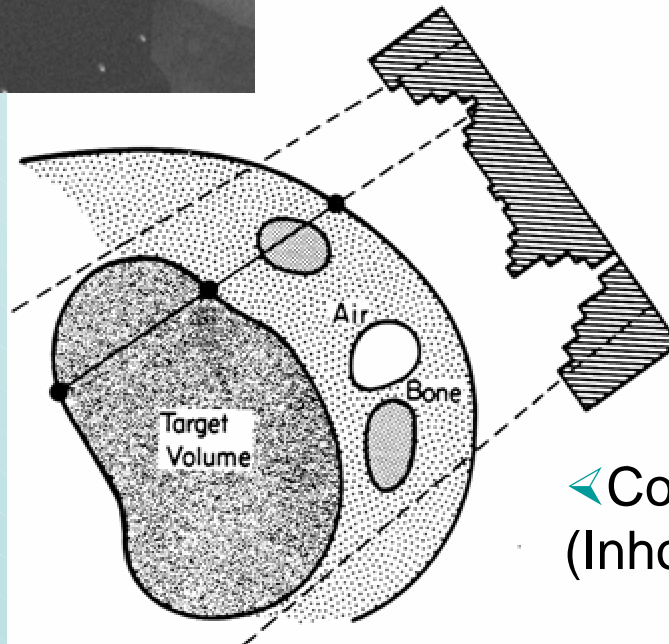
Conforming the Beam to the Target: Scattering Method



◀ Modulator
(Thickness)



▶ Collimator
(Shape)



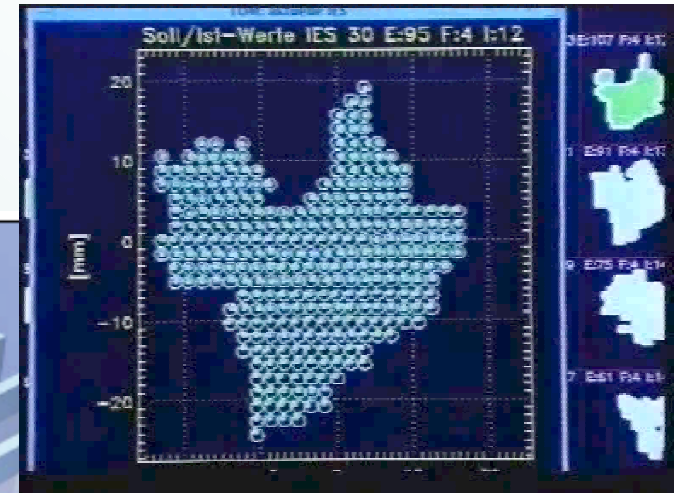
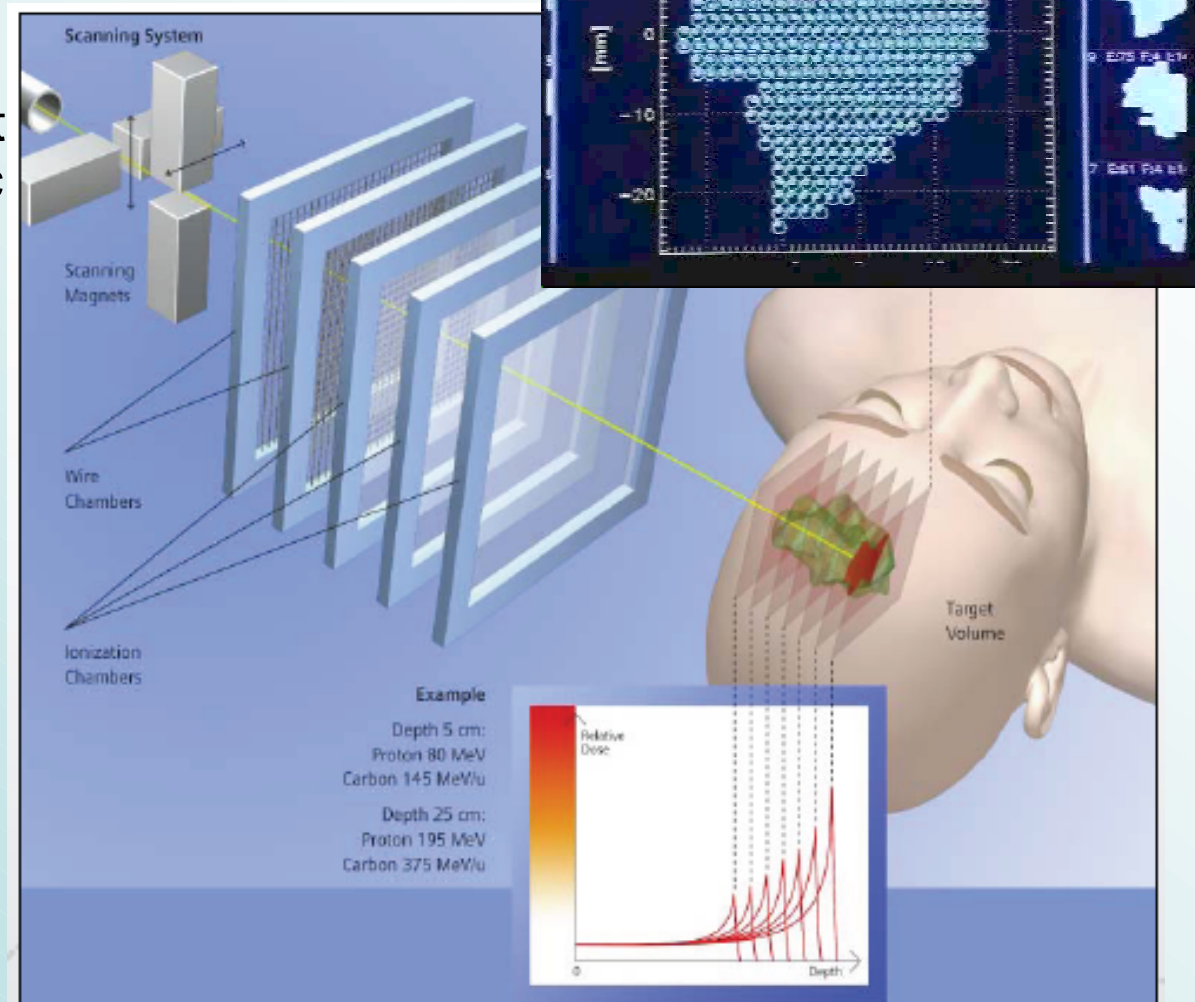
◀ Compensator
(Inhomogeneities)

Optimized Treatment By Beam Scanning

Development in the 90ies:
Scanning techniques

a) Protons (Pedroni PSI): spot scanning gantry (1D magnetic pencil beam scanning) plus passive range stacking (digital range shifter)

b) Ions (Haberer et al.): raster scanning (2D magnetic pencil beam scanning) plus active range stacking (spot size, intensity) in the accelerator



Intensity Controlled Raster Scanning with heavy charged particles:



Clinical Experience:

Protons:

PSI, CH: 450 patients

MDACC, MGH

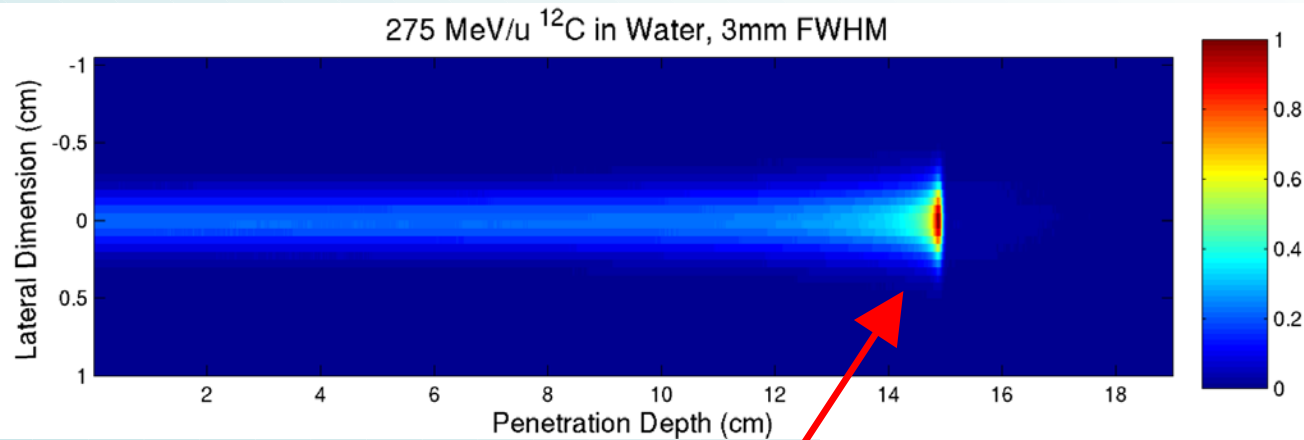
Carbon-ions:

GSI, D: 440 patients

Clinical Feasibility

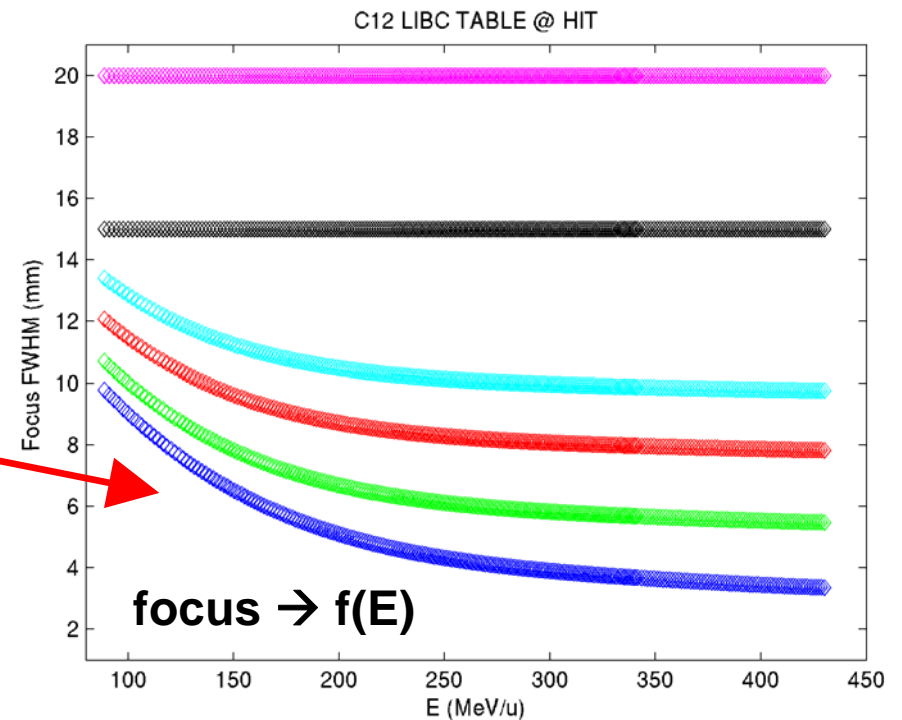
Verification film irradiated with C-12 in 1996

Challenge: Size Of The Beam, Precision, Time



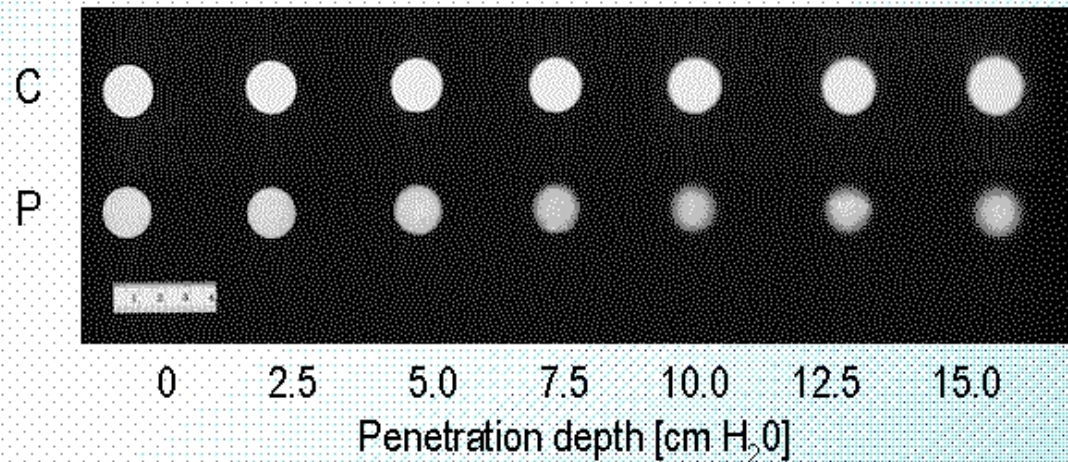
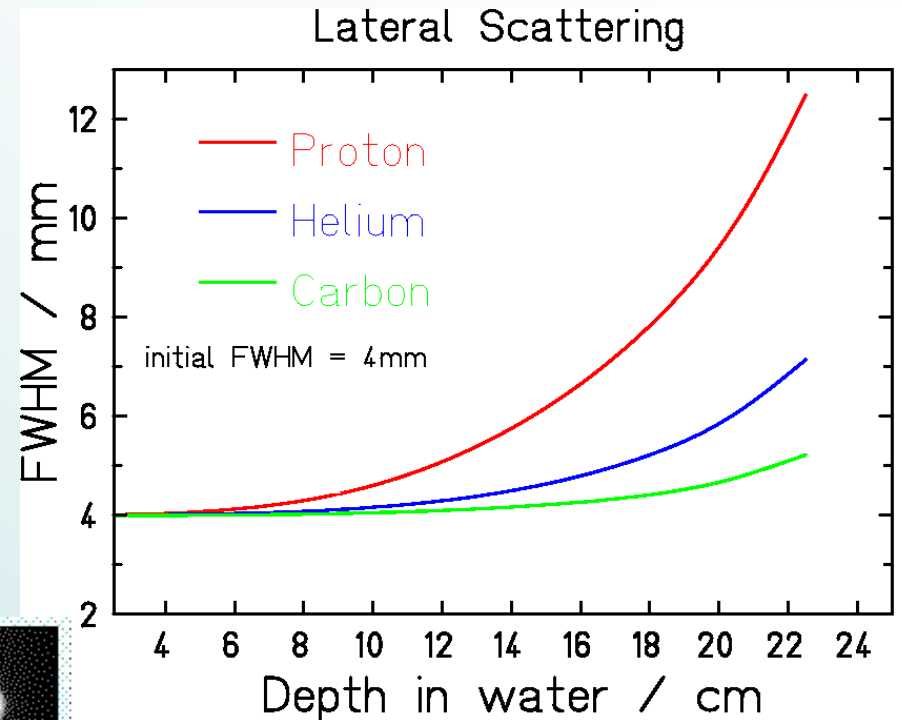
Straggling effects
must be taken into
account!

(vacuum window,
dose monitoring
system,...)



Beam Size

Higher local precision with carbon for deep-seated tumour treatment



RADIOTHERAPY TREATMENT OF EARLY-STAGE PROSTATE CANCER WITH IMRT AND PROTONS: A TREATMENT PLANNING COMPARISON

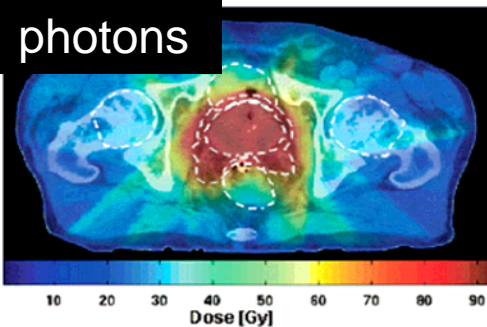
ALEXEI TROFIMOV, PH.D., PAUL L. NGUYEN, M.D., JOHN J. COEN, M.D., KAREN P. DOPPKE, M.S.,
 ROBERT J. SCHNEIDER, C.M.D., JUDITH A. ADAMS, C.M.D., THOMAS R. BORTFELD, PH.D.,
 ANTHONY L. ZIETMAN, M.D., THOMAS F. DELANEY, M.D., AND WILLIAM U. SHIPLEY, M.D.

Department of Radiation Oncology, Massachusetts General Hospital and Harvard Medical School, Boston, MA

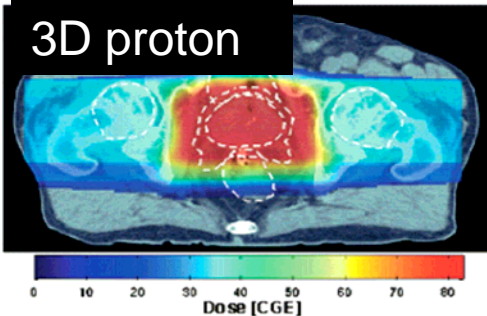
Table 1. Treatment plan objectives

Target prescription doses	
GTV (prostate)	100% to 79.2 Gy/CGE
CTV (GTV and seminal vesicles)	100% to 50.4 Gy/CGE
PTV2 (GTV + 5-mm margin)	98% to 79.2 Gy/CGE
PTV1 (CTV + 5-mm margin)	98% to 50.4 Gy/CGE
Tolerance doses for healthy organs	
Rectum	<50% to 60 Gy/CGE <35% to 65 Gy/CGE <25% to 70 Gy/CGE <15% to 75 Gy/CGE Maximum 84.7 Gy/CGE
Bladder	<50% to 65 Gy/CGE <35% to 70 Gy/CGE <25% to 75 Gy/CGE <15% to 80 Gy/CGE Maximum 84.7 Gy/CGE
Femoral head	Maximum 50 Gy/CGE
Penile bulb	Mean dose < 52.5 Gy/CGE

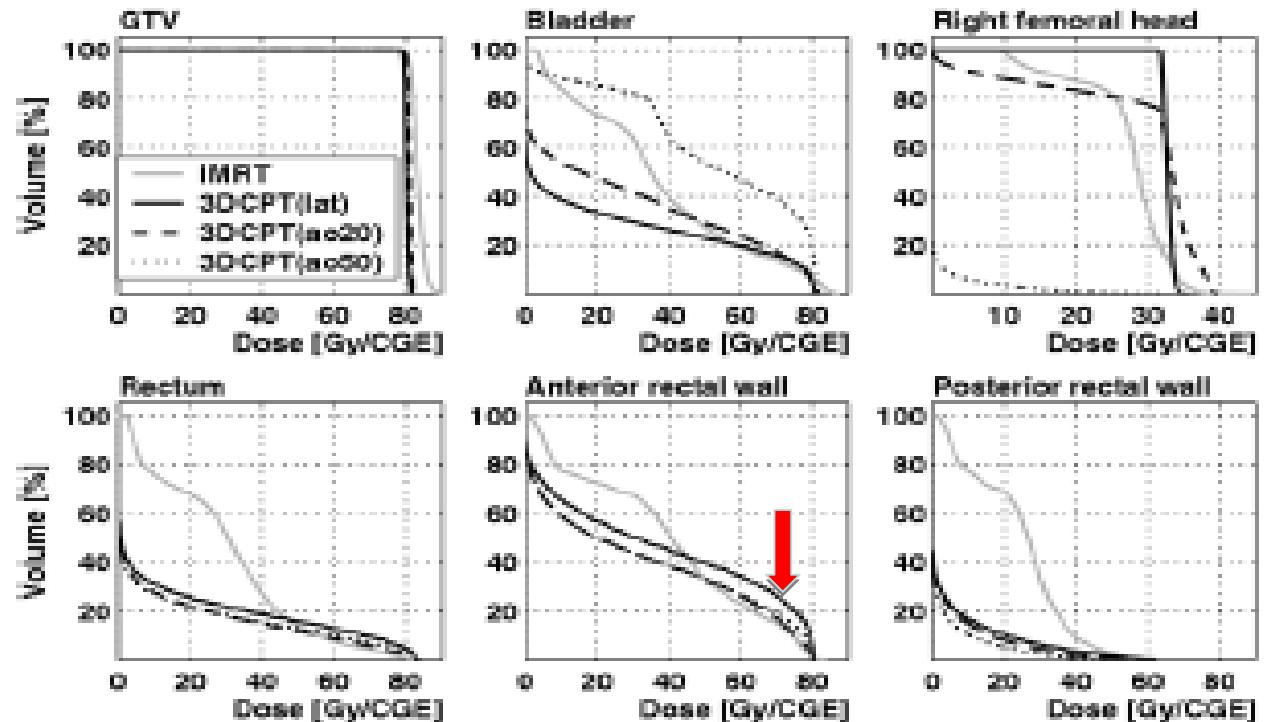
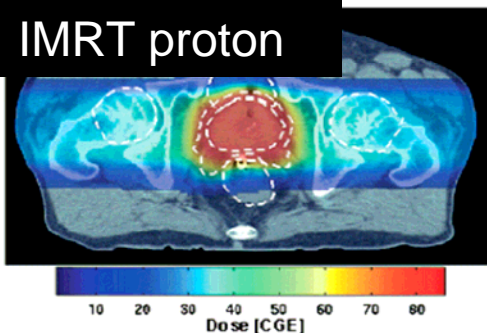
photons



3D proton



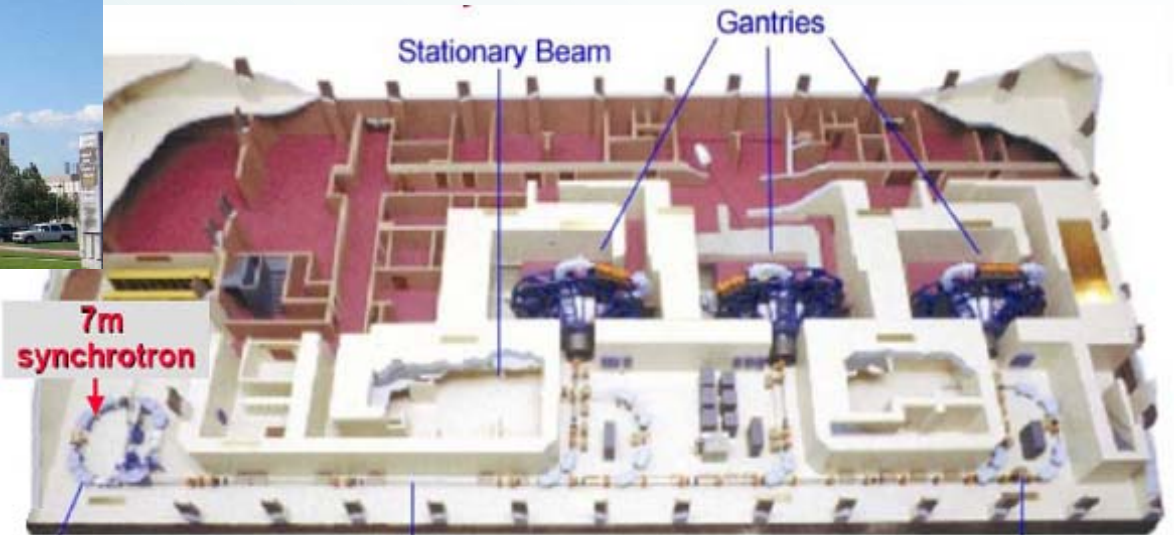
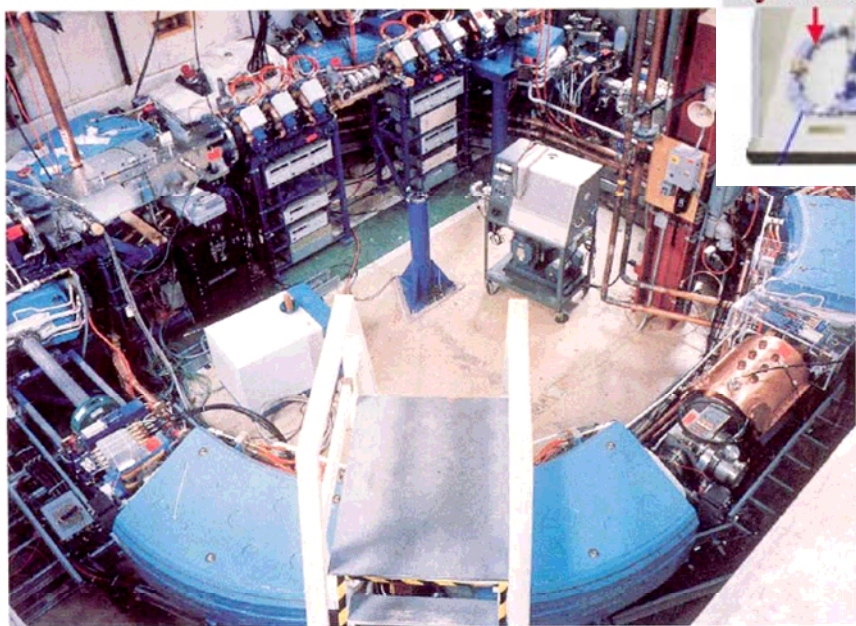
IMRT proton



First Hospital Based Particle Therapy Facility – Loma Linda/USA

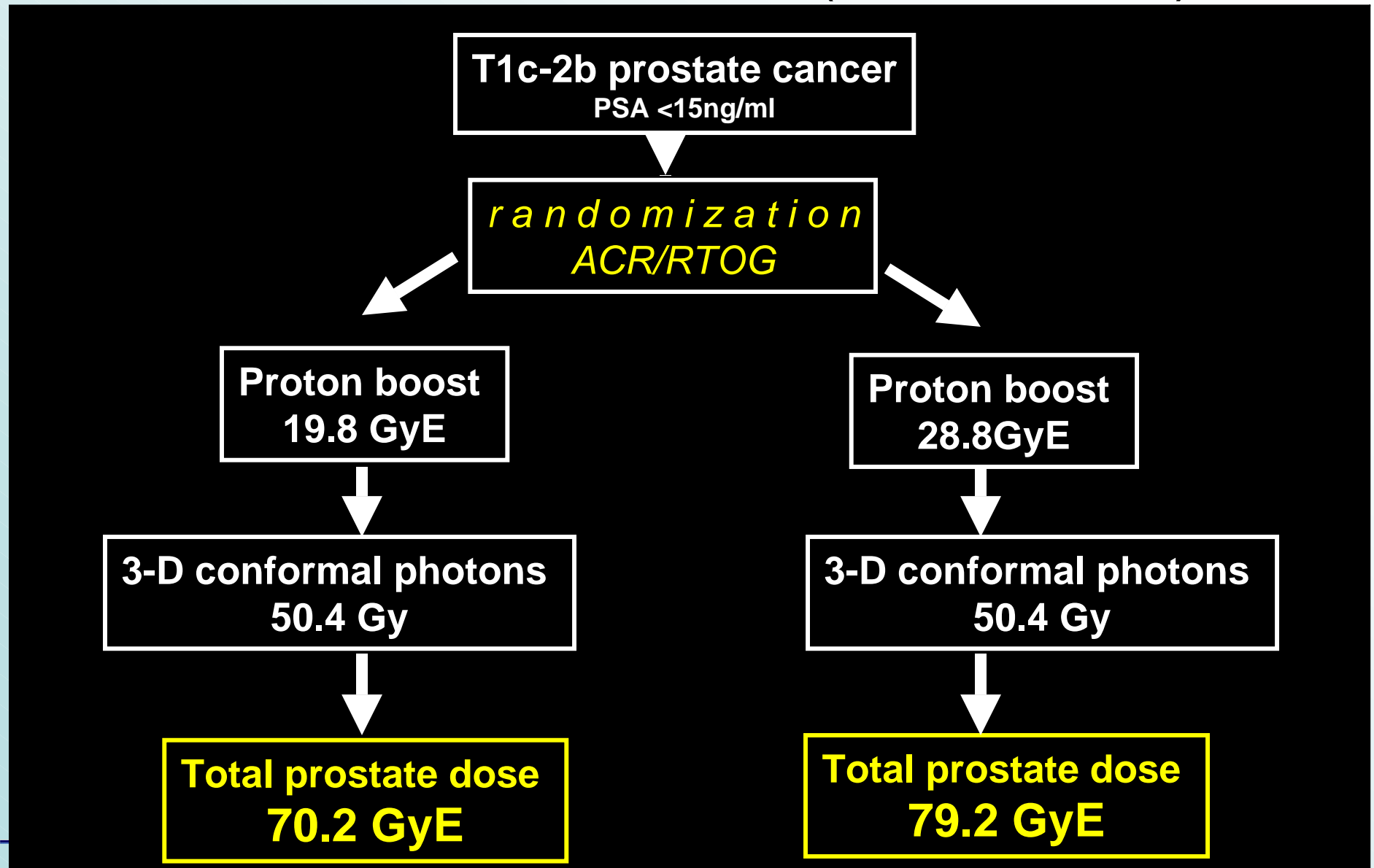


13,500 patients treated

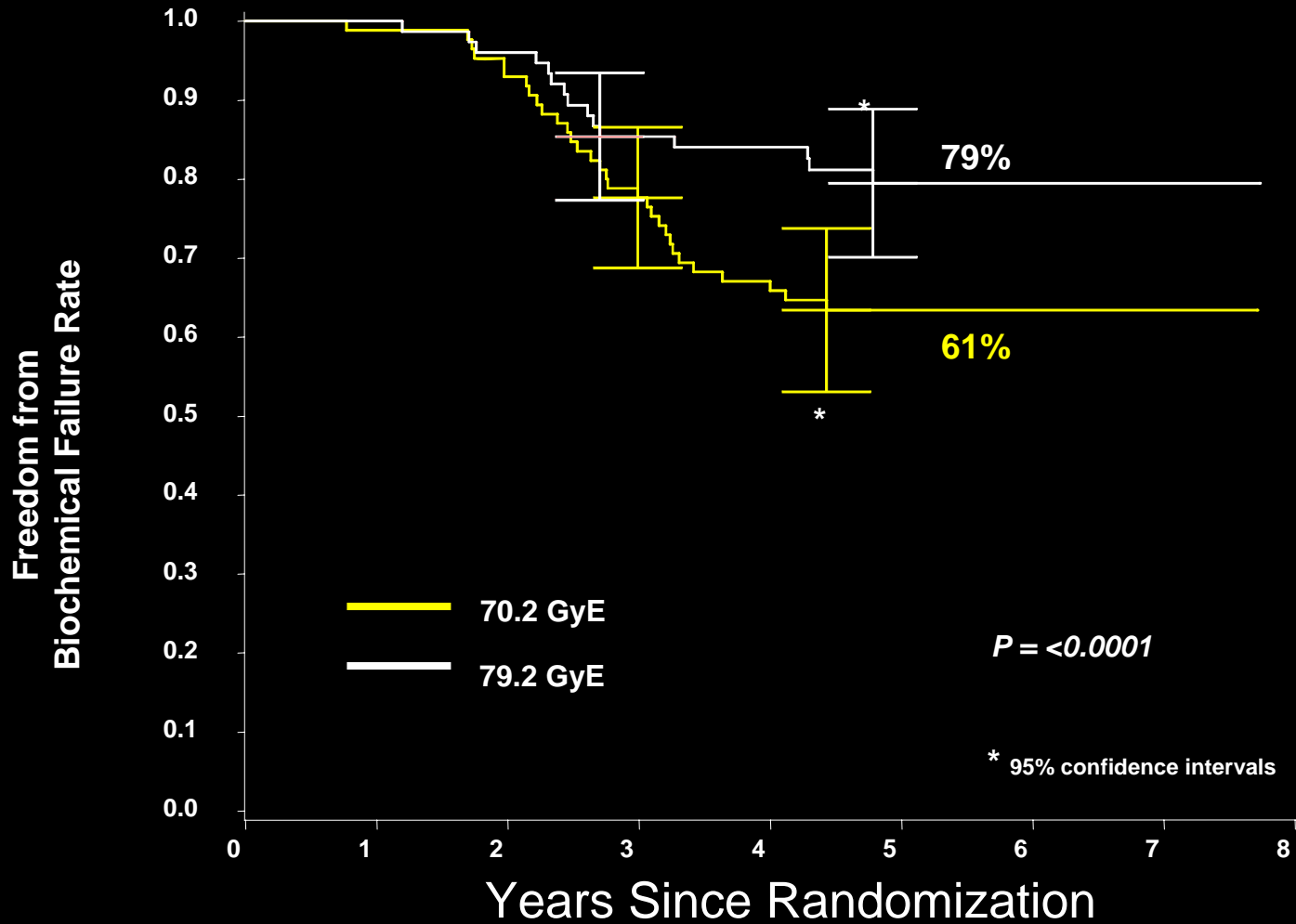


1st hospital based proton
therapy centre (since 1990)
using a synchrotron –
designed and commissioned
by Fermilab
2005: 160 sessions/day

Study Of Protontherapy In Patients With Prostate Cancer (PROG 9509)



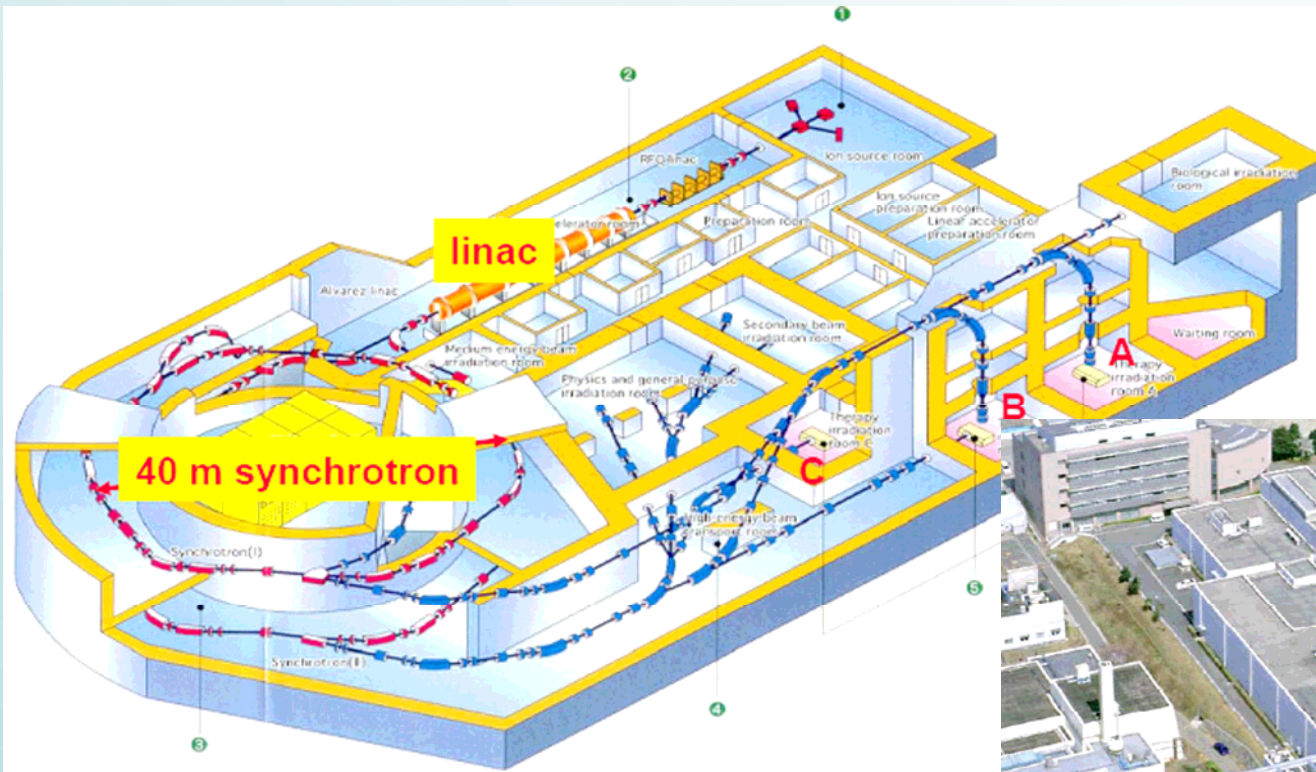
Improved Freedom from Biochemical Failure (PSA)



at risk

70.2 GyE	197	196	171	139	118	76	31	10	10
79.2 GyE	195	194	184	163	148	99	46	20	2

Particle Therapy Facilities – HIMAC/Japan



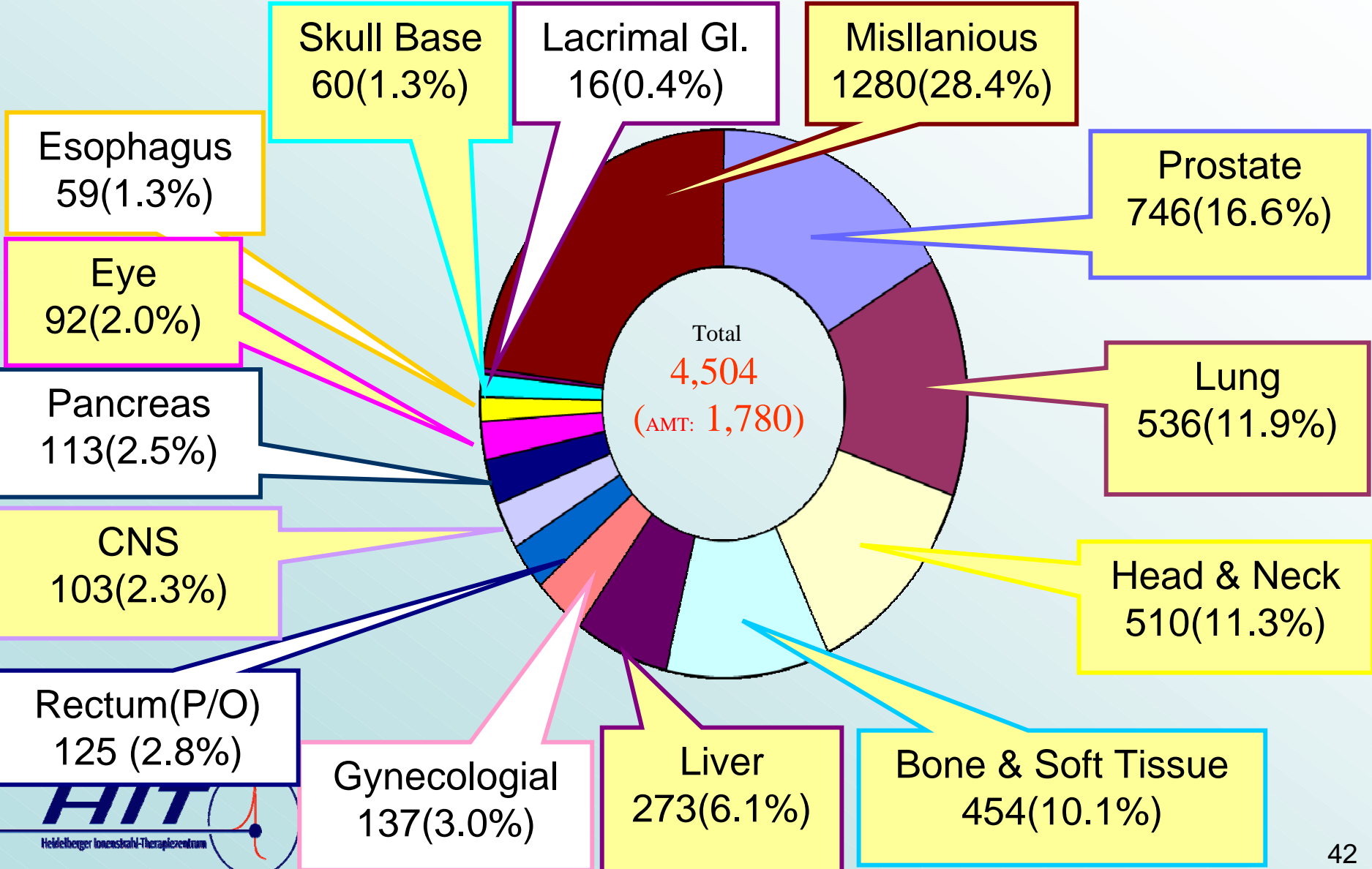
The Heavy Ion Medical Accelerator of NIRS (since 1994)



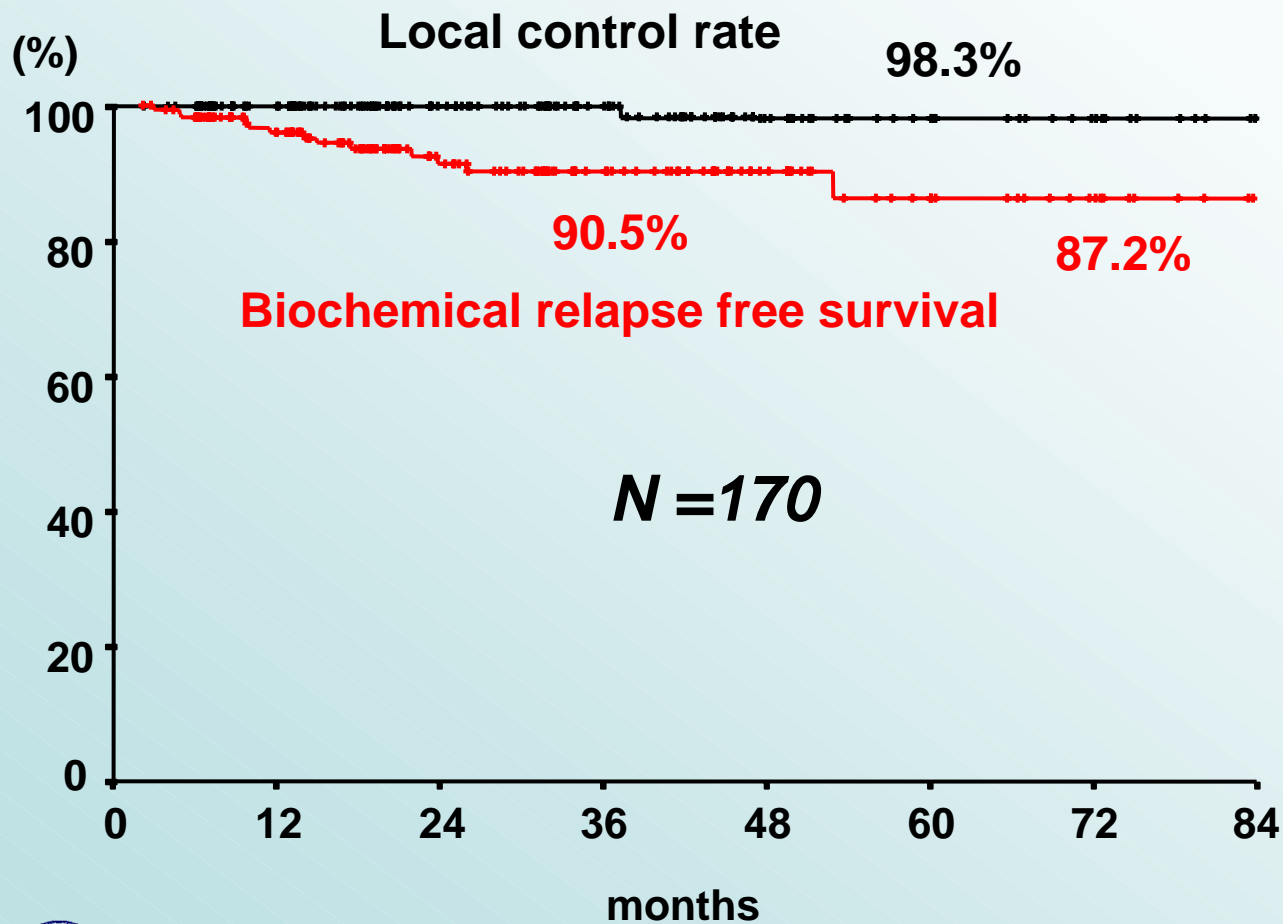
Two identical 800 MeV/u synchrotrons for ions up to Argon; mainly Carbon is used

4,500 patients treated

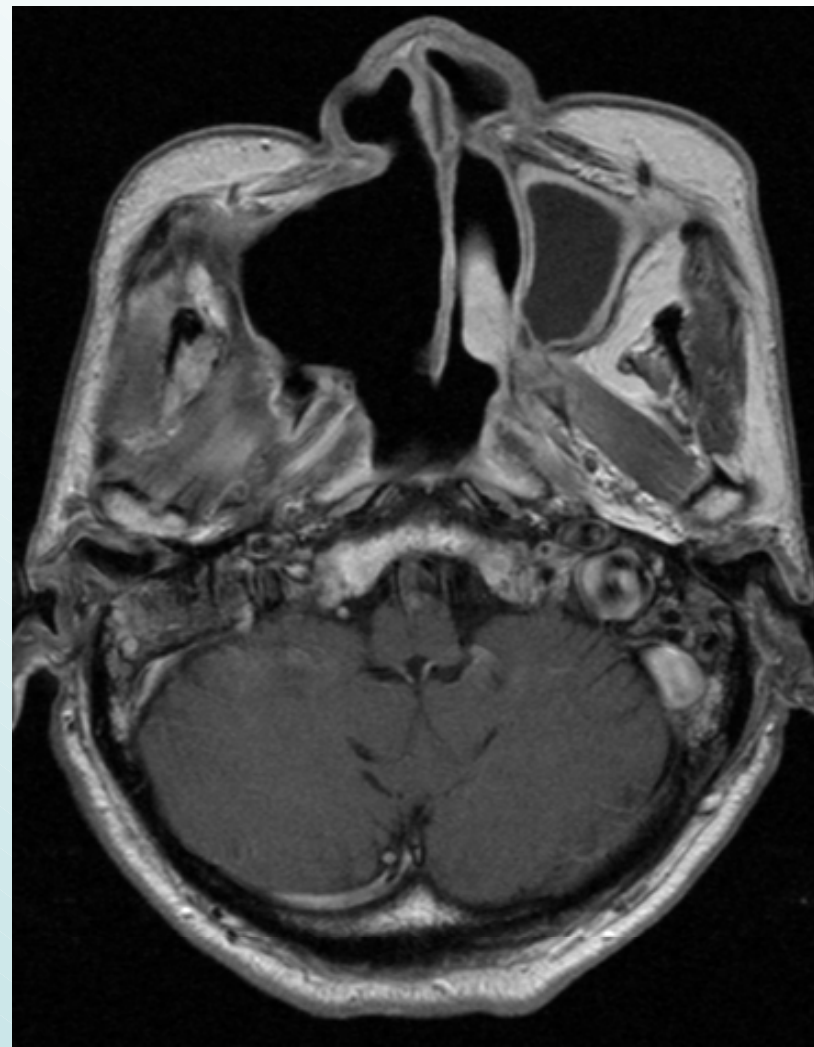
Patients enrolled into Carbon Ion Radiotherapy CHIBA (June 1994 ~ February 2009)



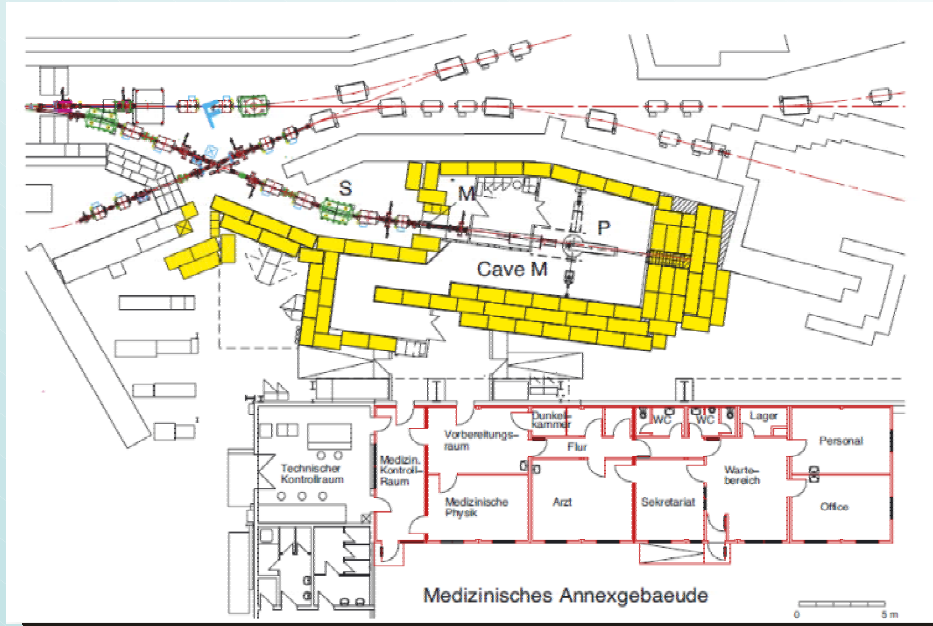
Local Control & Biochemical Relapse Free Rates Prostate Cancer (Japan)



Patient mit inoperablem malignen Melanom 57.6GyE/16fx



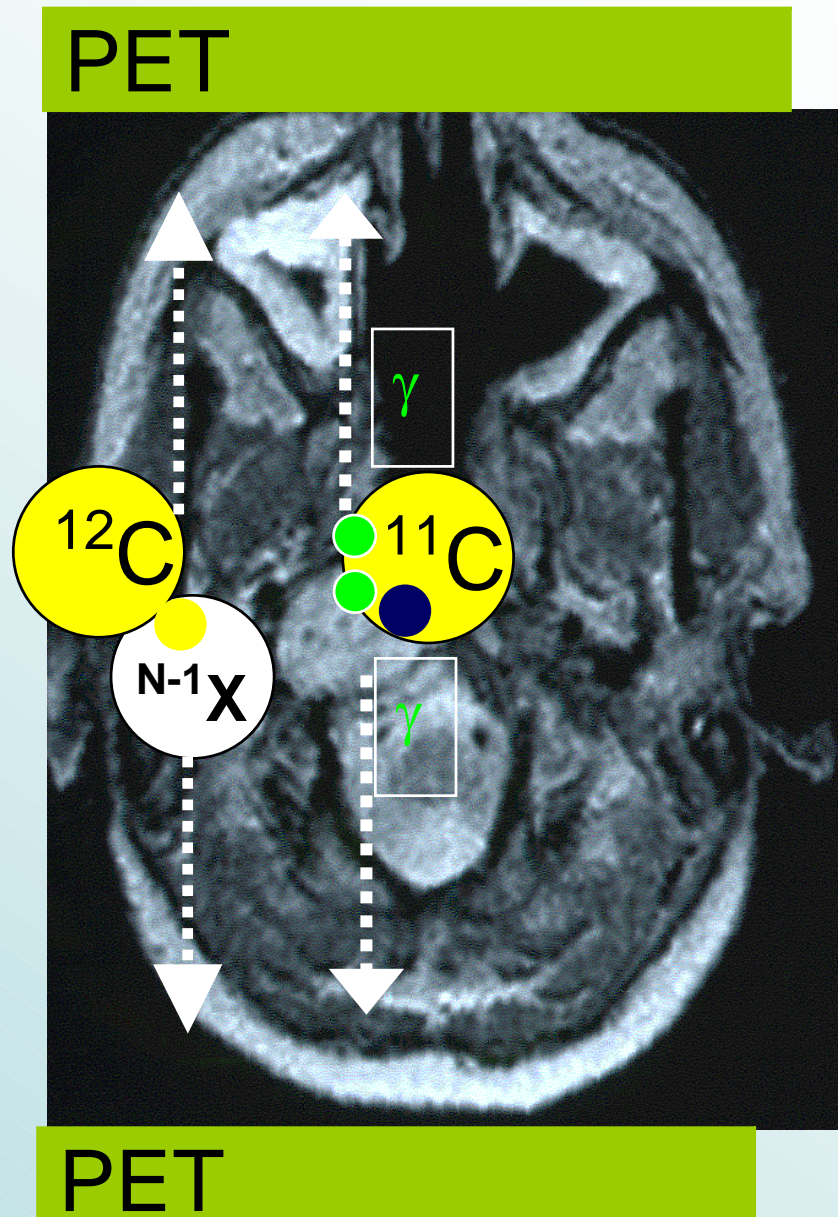
Particle Therapy Facilities – HIT/Heidelberg



HIT concept and layout is based on experience from GSI; 448 patients were treated with carbon beams from 1997 – 2008 using raster scanning technique



Principle of in-situ PET

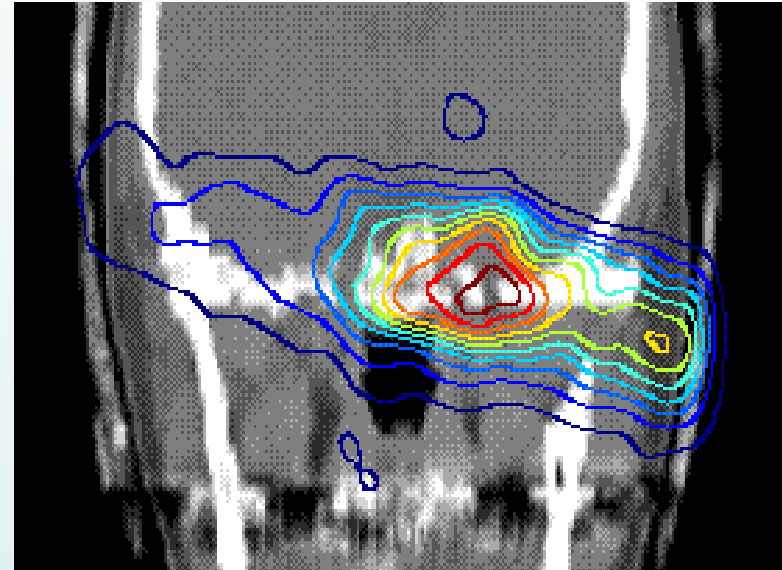


Verification with PET

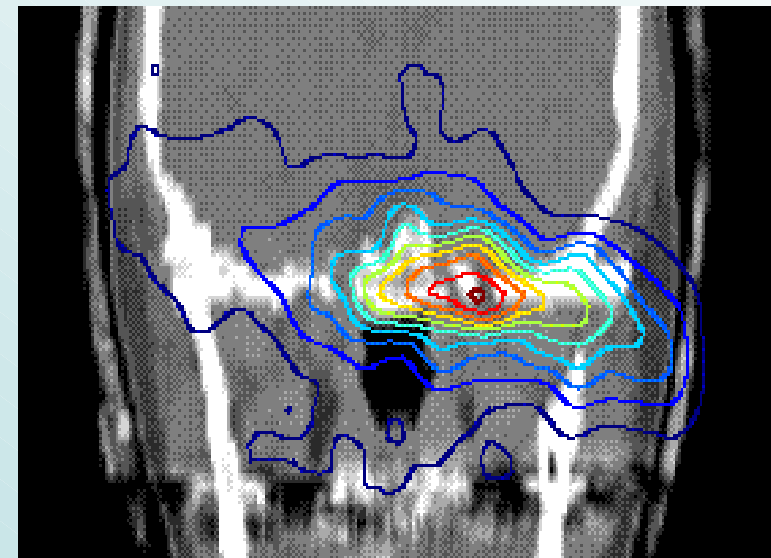


Patient during treatment

Expected PET

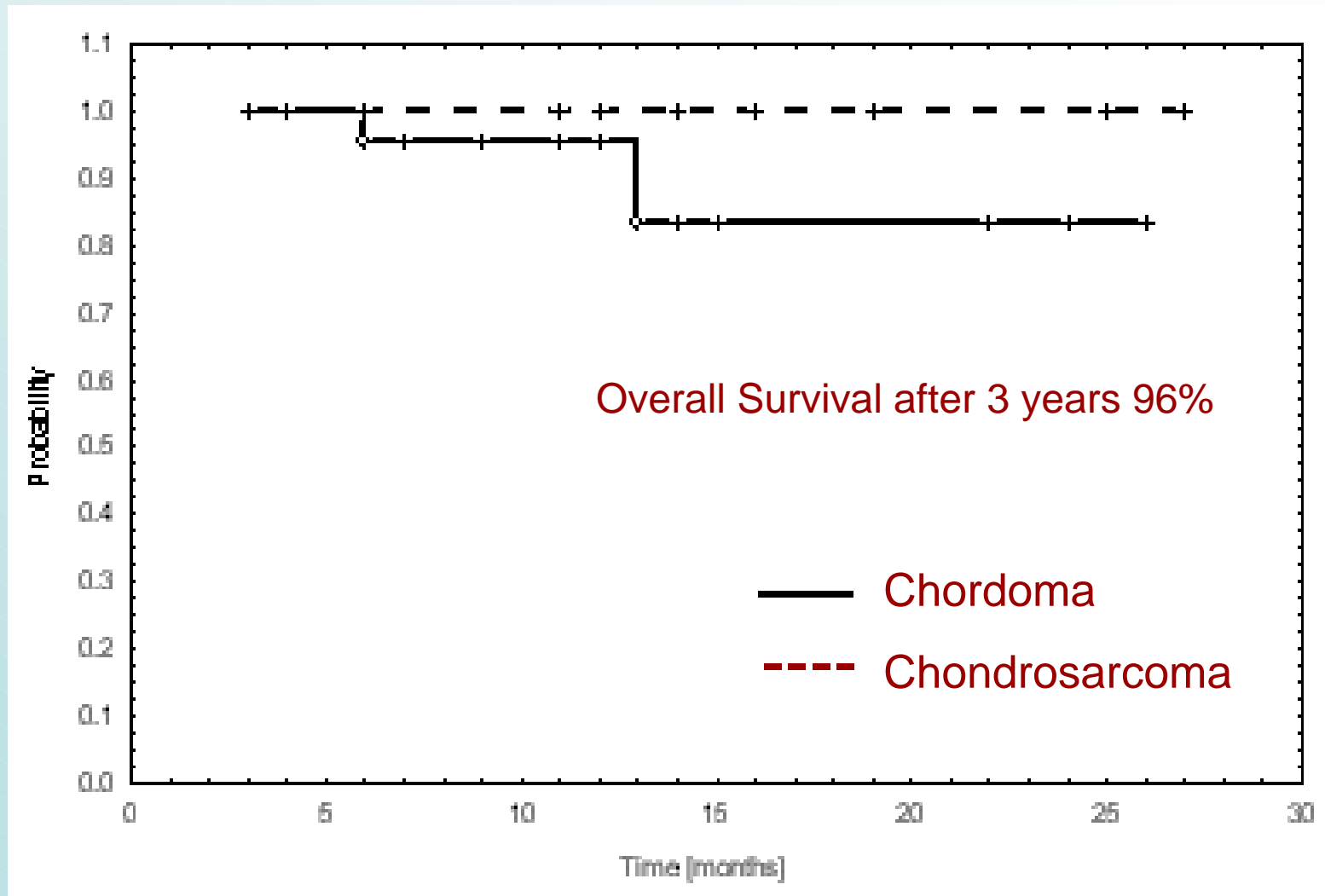


PET-Measurement



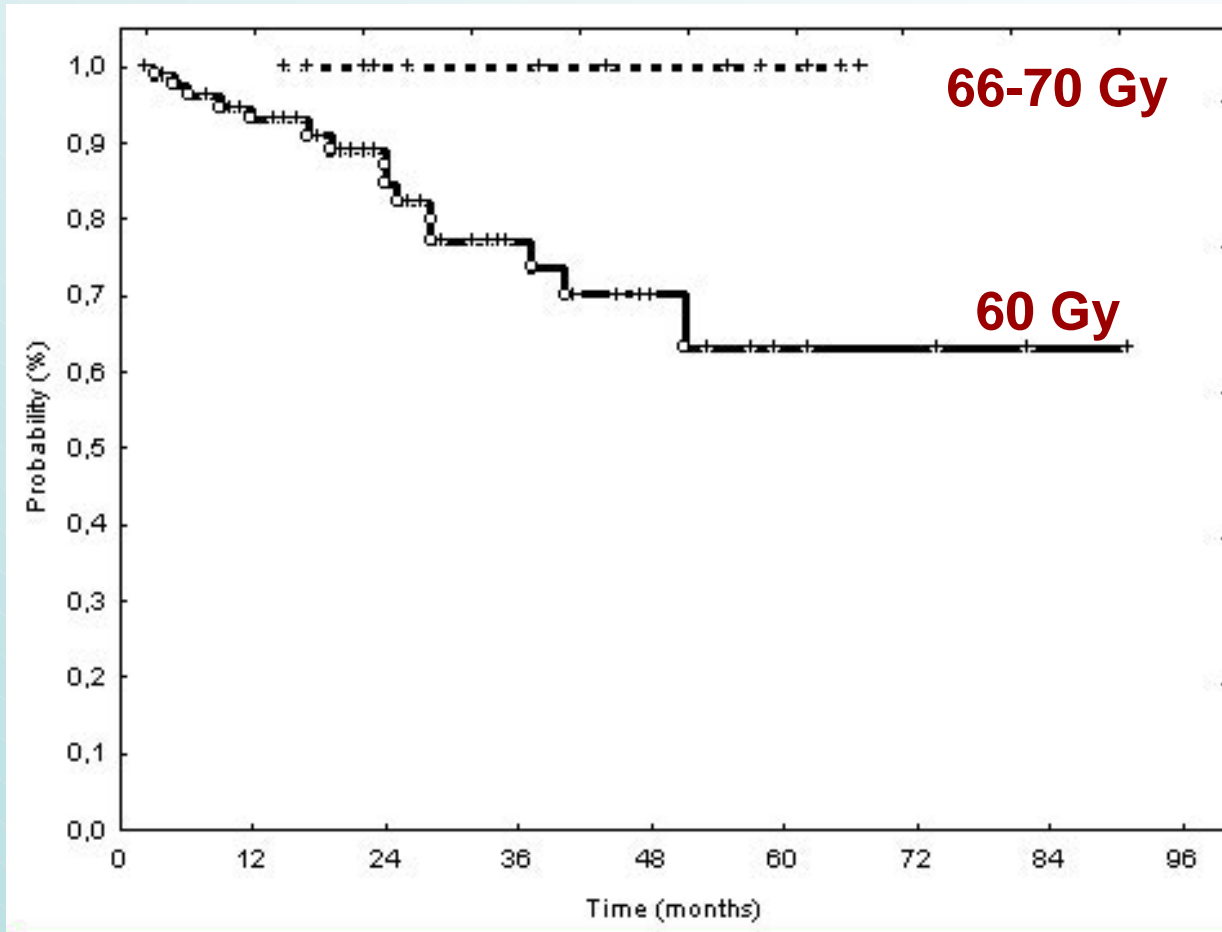
Progressionfree Survival

Chordoma / Chondrosarcoma G1/2 n=67 (Phase II Study)

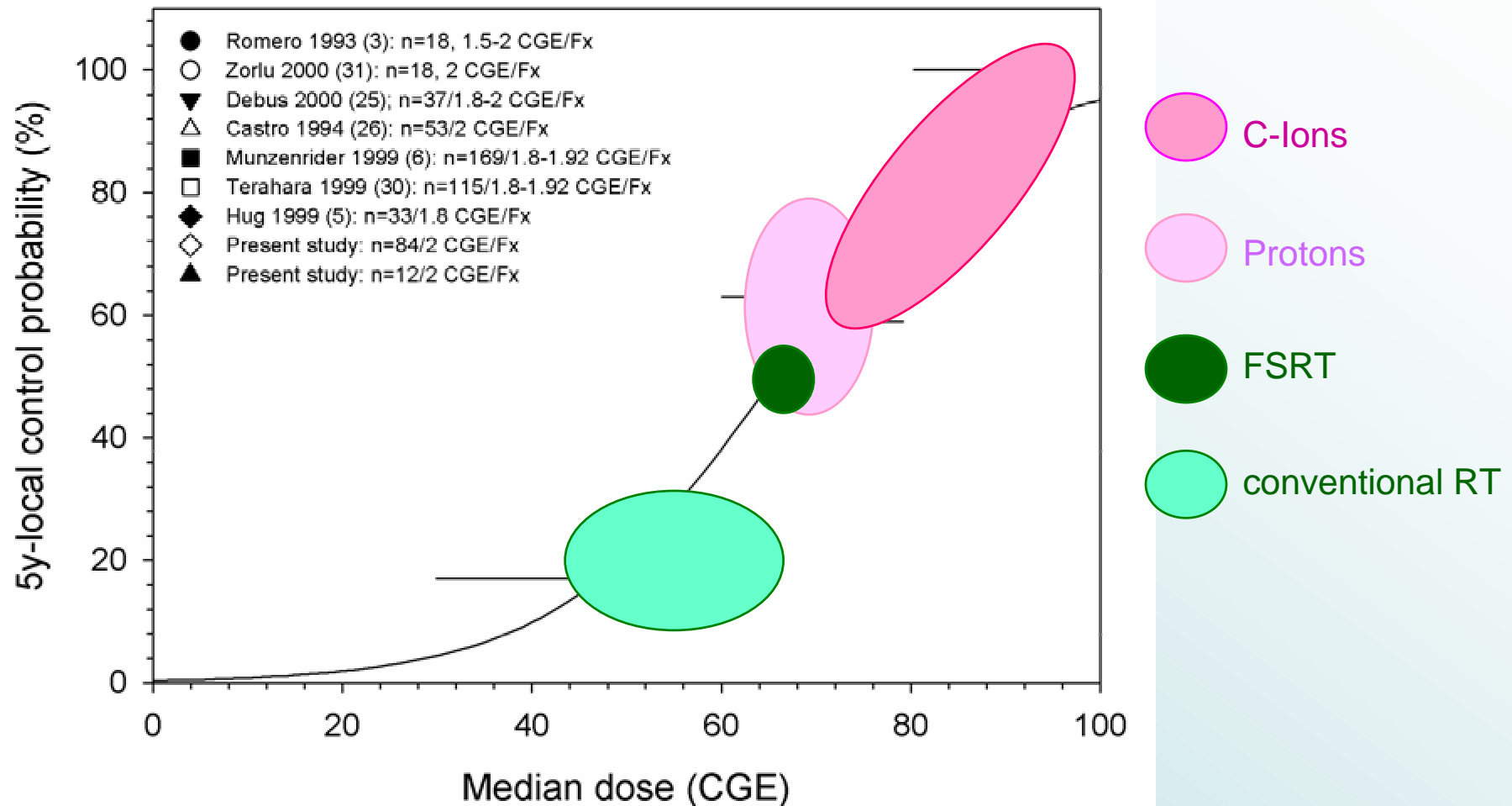


Local Tumor Control

Chordome n=91 (Dose =60 Gy vs > 60 Gy)

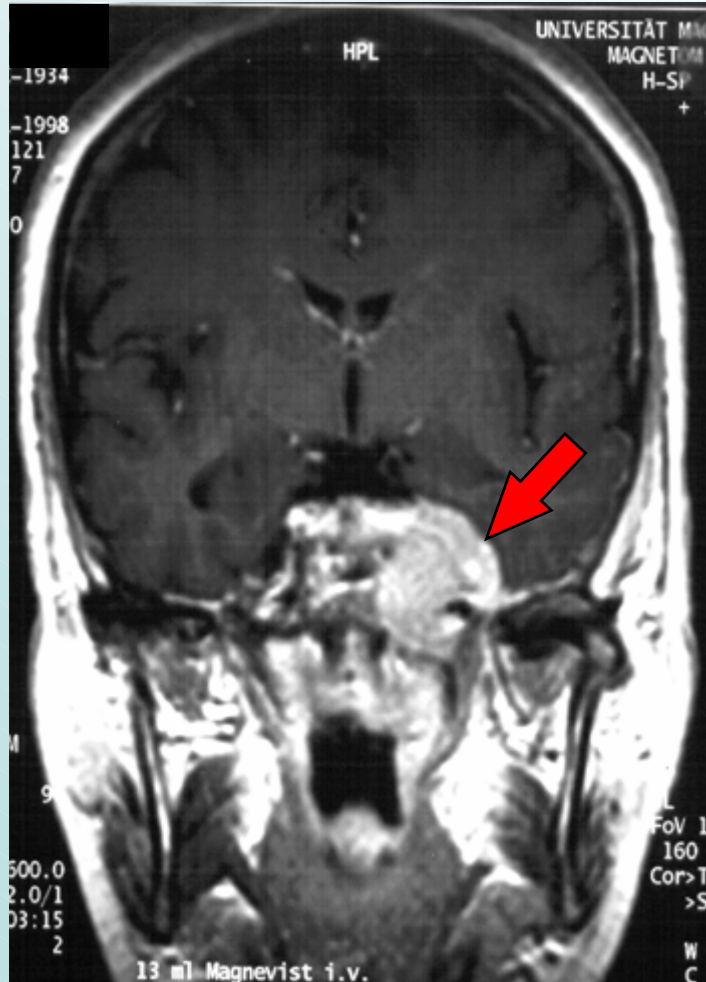


Motivation: Dose Response Relationship Radiotherapy of Skull Base Chordomas

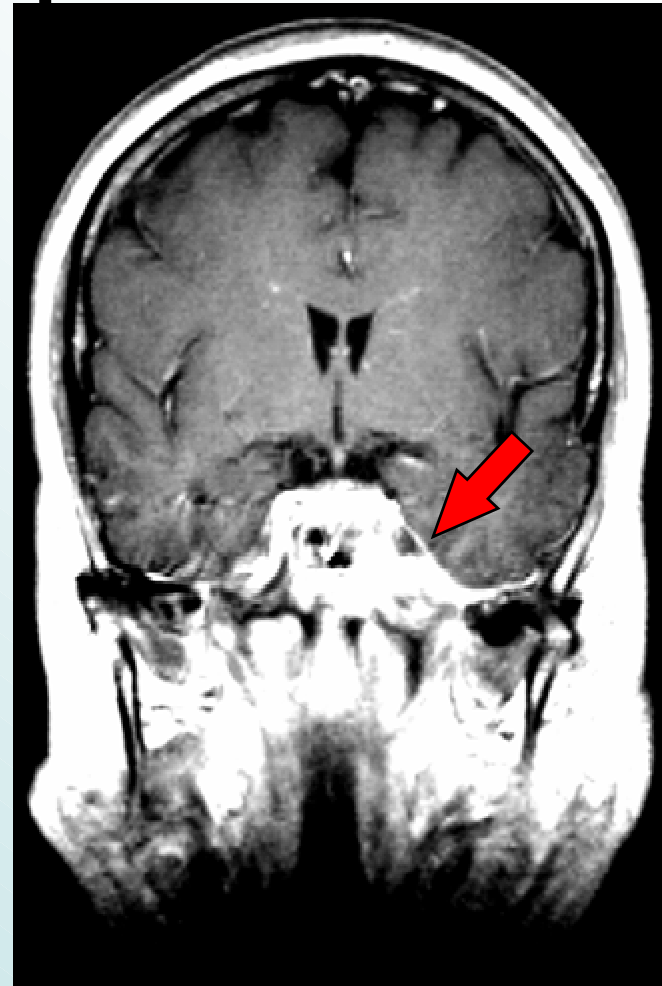


[Schulz-Ertner, IJROBP 2007]

Adenoidzystic Carcinoma: Follow-up



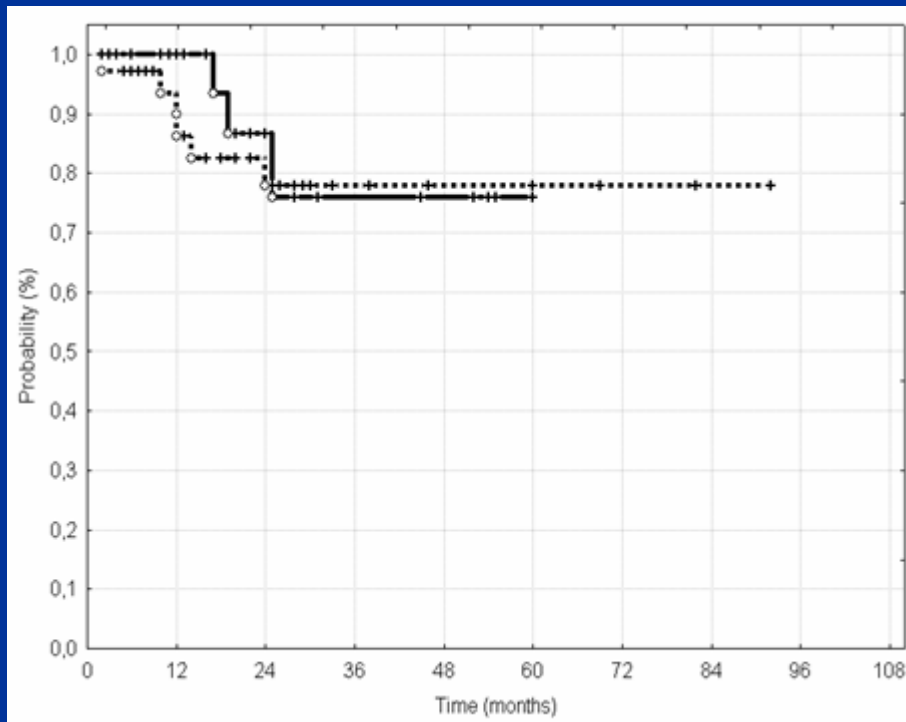
Before C12-RT



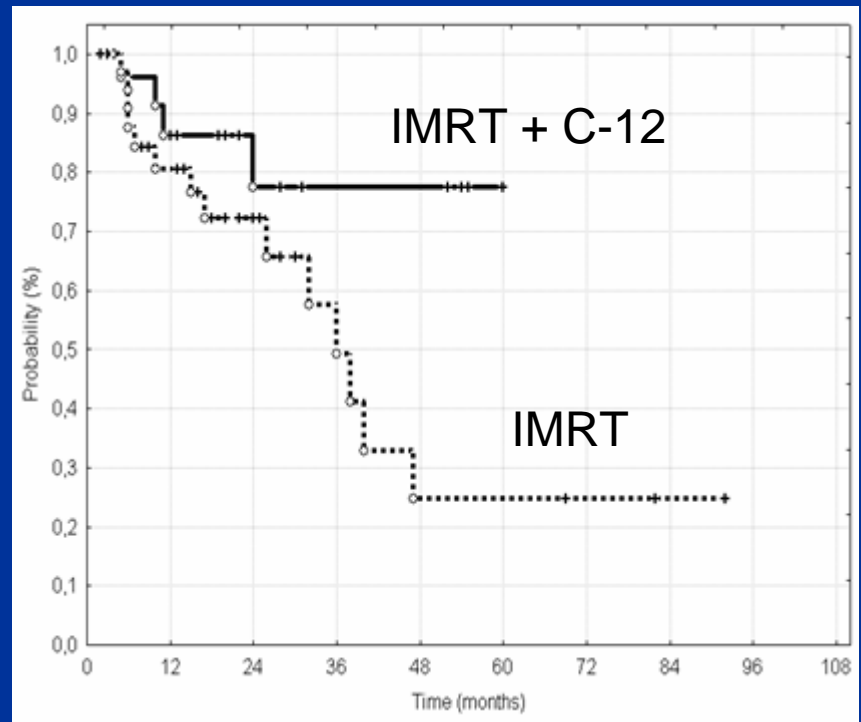
6 Weeks after RT

FSRT / IMRT vs. FSRT / IMRT + C12

locally advanced adenoidcystic carcinoma



Overall Survival



Local Control

- no dose limiting acute toxicity
- late toxicity > CTC grade 2 < 5%

Schulz-Ertner, Cancer. 2005 Jul 15;104(2):338-44

First Stone Ceremony Of HIT: May, 2004



Accelerator On Campus facilitating clinical and translational research

Strong partners joint forces @HIT: university HD, NCT, dkfz, GSI

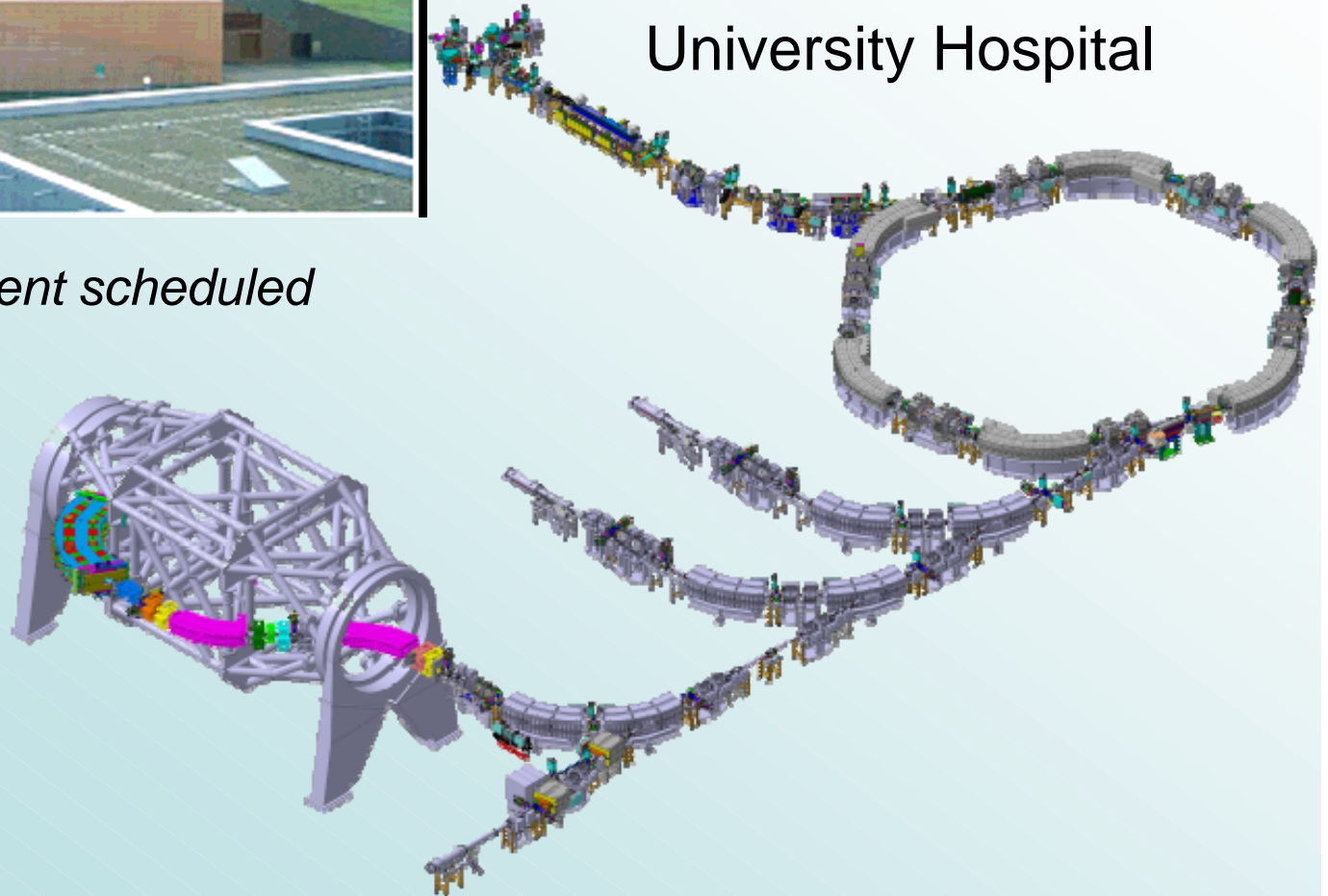


Particle Therapy Facilities – HIT/Heidelberg



Compact building (60 x 70 m², 3 levels), directly linked to the “Head Clinics” of the University Hospital

Start of patient treatment scheduled in 2 weeks



Particle Therapy Facilities – HIT/Heidelberg



Worldwide first isocentric ion gantry – including a scanning system:

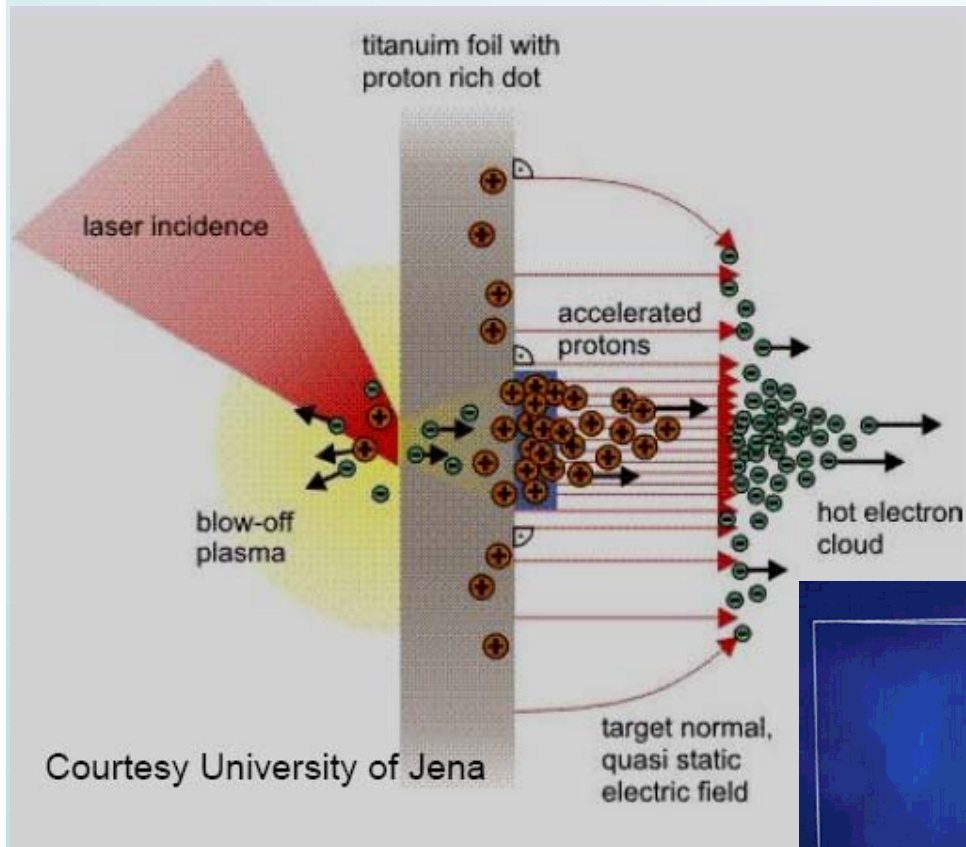
**Ø = 13m
25m long**

600 tons overall weight

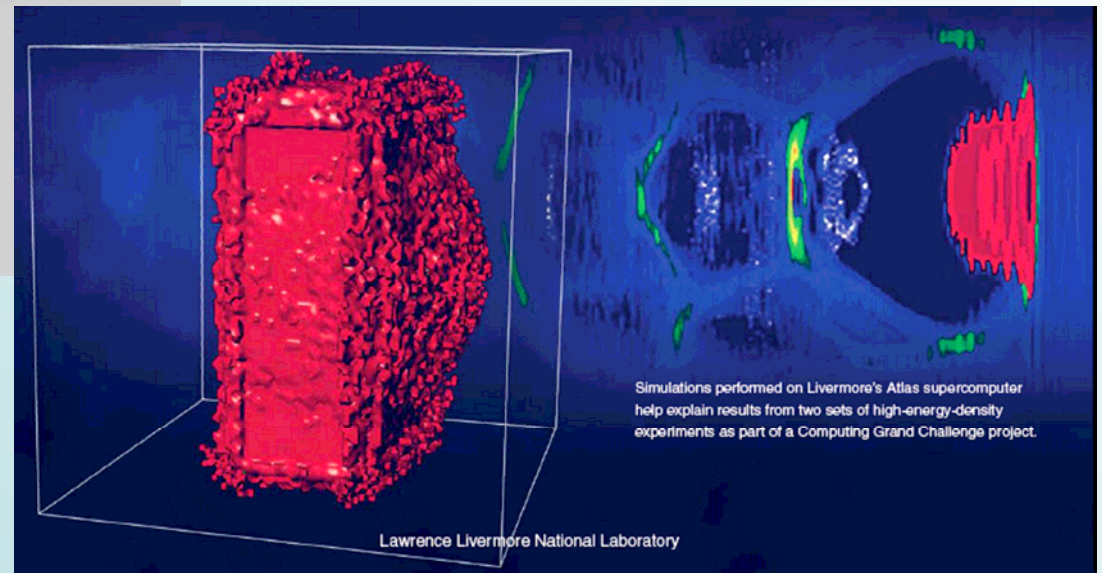
0.5 mm max. deformation



New concepts – laser plasma accelerators



- **Laser: 50 fs, 50 J (Petawatt!)**
- **$I = 10^{21}$ W/cm²**
- **10^{11} protons up to 300 MeV should be possible**
- **Repetition rate?**
- **Intensity control?**



New concepts – Dielectric wall accelerators

G. Caporaso et al, LLNL

250 MeV protons in 2.5 m?

Pulse-to-pulse energy & intensity variation

“Hoping to build a full-scale prototype soon”

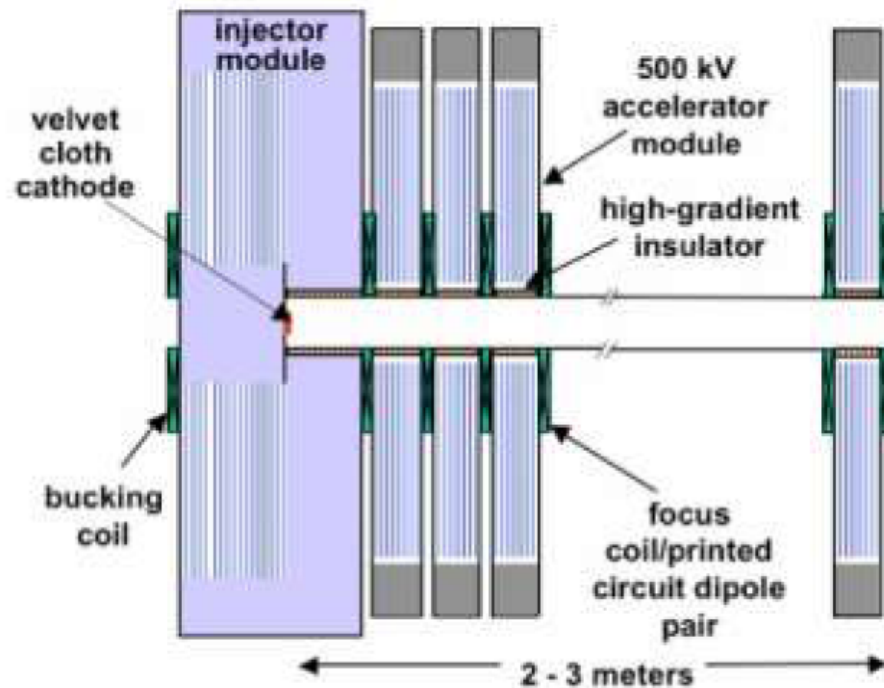
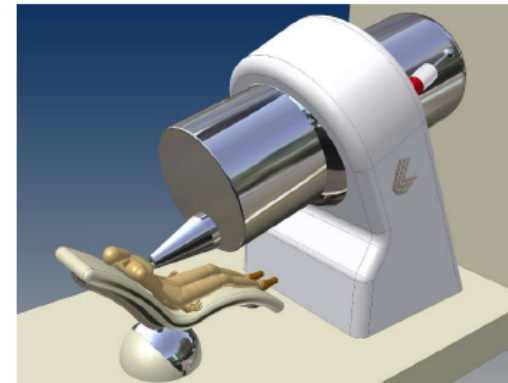
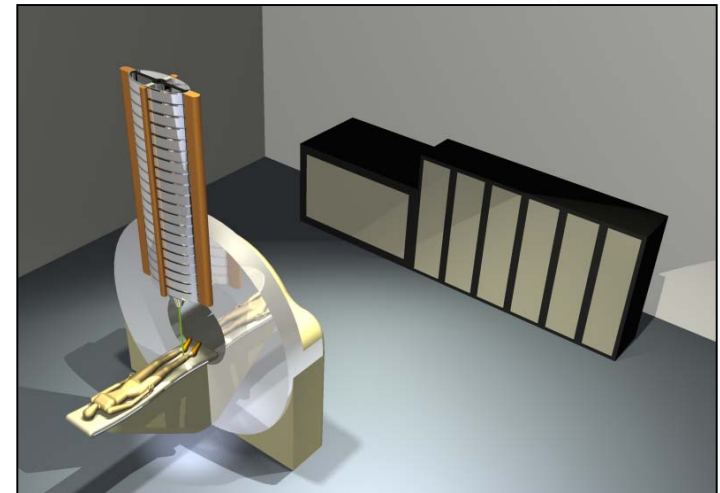
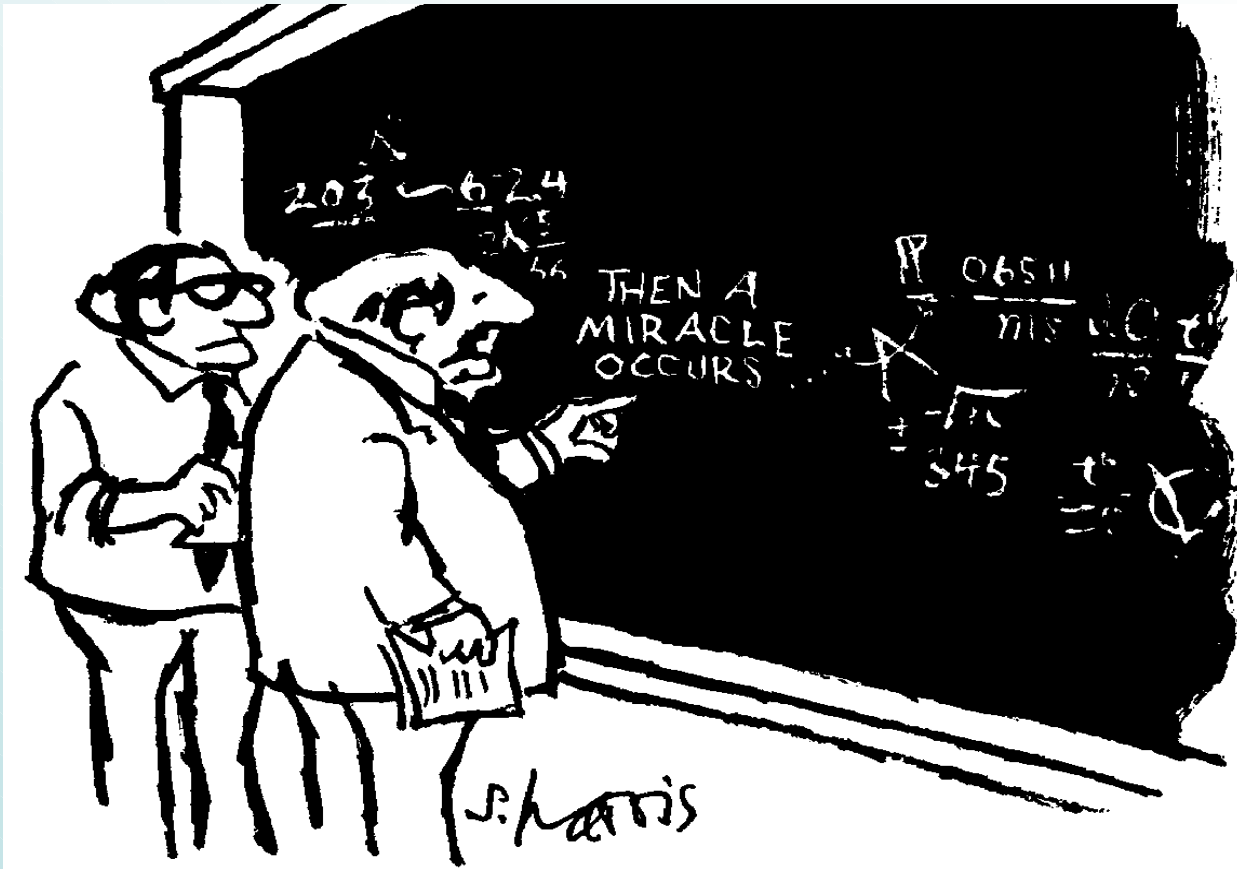


Figure 1: Dielectric wall induction accelerator configuration.



Conclusion

- Particle accelerators are an important and well established tool in medicine
- There has been considerable progress in recent years on the technical, biological and clinical knowledge
- Further research is warranted to fully exploit the advantages of charged particles with higher efficiency and at lower costs



"I THINK YOU SHOULD BE MORE EXPLICIT HERE IN STEP TWO."

Thank you for your attention!